

PATENT

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APPLICATION FOR UNITED STATES LETTERS PATENT
for
METHODS AND APPARATUS FOR PATHOGEN DETECTION, IDENTIFICATION
AND/OR QUANTIFICATION

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BACKGROUND OF THE INVENTION

[0001] The present application claims the benefit under 35 U.S.C. §119(e) of provisional Patent Application Serial Nos. 60/407,412, filed August 30, 2002; 60/422,439, filed October 19, 2002; 60/435,924, filed December 20, 2002; 60/435,934, filed December 20, 2002; 60/440,670, filed January 15, 2003; 60/451,107, filed February 27, 2003; and 60/470,347, filed May 13, 2002, entitled, "Nucleic Acid Detection and Quantification Using Terminal Transferase Based Assays" by Arjang Hassibi and Siavash Ghazvini. The text of each provisional application is incorporated herein by reference in its entirety.

Field of the Invention

[0002] The present invention relates to the field of pathogen detection. More specifically, the invention relates to methods, compositions and apparatus for cell or pathogen detection, identification and/or quantification. In particular embodiments of the invention, the methods may involve use of a bioluminescence regenerative cycle (BRC) and optical detection of bioluminescence.

Description of Related Art

[0003] Methods of precise and highly sensitive detection, identification and/or quantification of cells or pathogens are of use for a number of medical, epidemiological, public health, biological warfare and other applications. Traditionally, the detection and identification of pathogens has been an expensive and time-consuming process. Patients demonstrating clinical symptoms of an infection are generally diagnosed by analysis of blood or body fluid samples, using a variety of culturing and staining methods for identification of pathogen species (Prescott *et al.*, Eds., "Clinical microbiology," In *Microbiology*, 2nd ed., pp.672-679, Wm. C. Brown Publishers, Dubuque, IA, 1993).

[0004] Pathogens in clinical samples can be analyzed by various physical and biochemical characteristics, such as shape (rod-shaped or spherical), growth on special media and colorimetric characterization (gram-positive or gram-negative), or growth on selective media to determine the antibiotic resistance properties of the microbes. Each of these approaches requires a minimum number of microbes, normally much larger than the amount found in the original samples. Hence, the majority of these tests require culturing as a means of increasing the population of pathogens in solution. Once a sufficient number of the microbes have grown, the standard tests are performed. In certain cases, unidentified pathogens may be very difficult to culture under standard conditions, making identification difficult.

[0005] The standard bacterial assays are largely based upon gross visual identification and it is generally difficult to determine the exact species of the infecting microbe. In addition, the culture process can take from days to weeks, depending on the pathogen's growth characteristics. In most cases, the physician initiates treatment prior to receiving laboratory diagnosis and later modifies treatment appropriately when the test results become available. By the time an infectious pathogen has been identified and its drug-resistance profile determined, it may be too late for the patient. For example, in the United States, over 2 million individuals suffer from hospital-acquired infections, which may result in bacteremia and in some cases severe sepsis (Datamonitor, "Antimicrobial resistance: Resistance drives a mature market," Brief No. BFHC0348 2001 <www.datamonitor.com>). Sepsis is the 11th leading cause of death overall in the U.S. resulting in over 500 deaths per day (Angus *et al.*, *Crit Care Med* 29:1303-1310, 2001). As with any other disease condition, early identification, typing and treatment monitoring can be the key that decides between a good or bad prognosis.

[0006] A major problem with differential growth and staining techniques is that a specific organism may be detected in the presence of large quantities of other organisms. A number of tests are then needed to refine the identification of the bacterium. Typically colonies are subjected to supplementary identification tests, including microscopic, biochemical, immunological and/or genetic analysis. The extra tests increase the time and cost. Additionally, the need to detect pathogens in food, water and clinical samples such as blood, urine, saliva and fecal samples, where interfering components may hinder growth or assay methods have posed new problems for the traditional technologies and for more modern methods, such as polymerase chain reaction (PCR®) amplification.

[0007] Biochemical tests may be conducted using kits such as the API strip (Biomérieux Vitek) or PetrifilmTM (3MTM). Generally, culturing is still necessary prior to performing these and other streamlined biochemical tests. The API strip consists of 20 miniature tests contained in wells of a strip. The test is based on the metabolism of the organism and therefore can take from 8 to 24 hours, depending on the exact test. The use of kits for such identification has simplified the identification procedures, but the cost of each test is high and it remains a time consuming process.

[0008] To provide early identification of microbial infections, such as bacteremia and sepsis, methods based on unique antigens and nucleic acid sequences have been developed that identify specific molecular features of the pathogen. ELISA based methods rely on the

specific interaction of an antibody directed against microbial surface antigens. Several recent reports have disclosed immunosensors for pathogen detection based on ELISA and bioluminescence (Koch *et al.*, *Biosensors and Bioelectronics* 14:779-784, 2000; Premkumar *et al.*, *Talanta* 55:1029-1038, 2001; Squirrell *et al.*, *Analytica Chimica Acta* 457:109-114, 2002; Yacoub-George *et al.*, *Analytica Chimica Acta* 457:3-12, 2002). Although ELISA can be useful in identifying microbial isolates with speed and in a high-throughput manner, the reported sensitivity ranges from 10^3 - 10^7 colony-forming units per milliliter (Koch *et al.*, 2000; Yacoub-George *et al.*, 2002; Ruan *et al.*, *Anal Chem* 74:4814-4820, 2002). This level of sensitivity is insufficient to detect pathogens early in infection, without a culture step. This can result in "false-negatives" where even though an antigen is present in the sample, the levels are not high enough for detection. Ways to avoid these false-negatives include culturing samples to allow for additional growth of pathogens and subsequently increasing the abundance of antigen targets. However, this requires additional time (at least 24 hours) before the test results can be obtained, delaying accurate detection and identification of pathogens. Additionally, the effectiveness of immunoassays may be compromised because of a microbe's ability for altering surface antigenicity. Similarly, other tests that measure the titer of antibodies in patient's blood cannot distinguish current ongoing infections and past infections.

[0009] More sensitive methods have been developed that rely on identification of microbes by using their genetic material. The best-known nucleic acid detection assay is PCR. Pathogen nucleic acids are amplified using oligonucleotides that hybridize to the unique sequence of the pathogen DNA. Using fluorescence and size discrimination of the amplified product on an agarose gel, the technician can determine the existence of infection and its identity. Use of PCR-based assays can increase sensitivity, with amplification obtainable from bacterial target numbers ranging from 10^0 - 10^2 (Kong *et al.*, *Water Research* 36:2802-2812, 2002; O'Mahony *et al.*, *Journal of Microbiological Methods* 51:283-293, 2002; Papadelli *et al.*, *International Journal of Food Microbiology* 81:3 231-239, 2002). However, problems exist with PCR detection of pathogens. The sample processing required for PCR is time consuming and complicated, requiring trained technicians. False-positive rates and contamination are major issues due to the sensitivity of the assay. Similarly, point mutations within the sequence to which one or more of the oligonucleotides hybridize can lead to false-negative readings. Multiplexing is not practical, requiring multiple reactions to detect unknown pathogens. Also, in certain bacteria the genetic variation from drug-sensitive to

drug-resistant can be as small as a single nucleotide change. Even if an appropriate band is detected, there may be a need for sequencing to determine which isolate is present. Finally, if one assumes that either test (ELISA or PCR) can achieve a specificity of 99.9% in a screening of one million individuals (potentially due to biological warfare agent spread in a city), it is possible to misdiagnosis 1000 people that can potentially infect others.

[0010] Prophylactic use of broad-spectrum antibiotics as a stop-gap measure during bacterial culture and identification has suffered from the rapid development of bacterial strains that are resistant to most available antibiotics. Conversely, identification of the type of pathogen involved in an infection is required in order to prescribe narrow-spectrum antibiotics that are effective against particular bacterial strains. A need exists in the art for rapid, highly sensitive and specific methods for the differential diagnosis and identification of pathogens. A method by which detection and identification of bacterial pathogens can be achieved with a high degree of sensitivity, selectivity, rapidity, and accuracy is greatly needed. The present invention concerns a novel approach of immunocapture detection of pathogens, followed by nucleic acid based confirmation in a homogenous serial assay.

SUMMARY OF THE INVENTION

[0011] The present invention fulfills an unresolved need in the art by providing methods for accurately detecting, identifying, quantifying and/or sequencing target cells or pathogens, such as bacteria. In preferred embodiments, the number of target cells or pathogens in a sample may be accurately determined over a seven order of magnitude range. The disclosed methods provide increased sensitivity and accuracy of target cell or pathogen detection, identification and/or quantification compared to prior art methods. Other advantages include lower cost, decreased use of toxic chemicals and avoidance of radioisotopes, decreased sample preparation and more rapid analysis.

[0012] In certain embodiments of the invention, the methods may comprise obtaining at least one sample suspected of containing one or more target cells or pathogens. Immunocapture techniques may be used to bind and immobilize pathogens of interest, for example using a pathogen-specific or pathogen-selective antibody attached to a magnetic bead or other solid surface. For example the surface may be the wall of a microfluidic channel in a solid matrix, such as a glass, quartz, semiconductor, or plastic chip or other solid surface. Alternatively, the surface may be the interior walls of a capillary tube including that made of glass, quartz, semiconductor, or plastic (polymeric) materials. Antibodies may be either monoclonal or

polyclonal, although monoclonal antibodies are preferred. In some embodiments, pathogen-specific antibodies may be attached to distinct areas of a chip so that detection of a signal from that location indicates the presence of target microbes in the sample.

[0013] Immunocapture of a target pathogen may be followed by cell lysis and detection of the pathogen nucleic acid, for example by BRC. In some embodiments, the pathogen nucleic acid may be detected by hybridization to a pathogen specific primer, followed by nucleic acid polymerization. The system has extremely high sensitivity (i.e. extremely low limits of detection). For example, BRC may be utilized for ultra-sensitive detection of microbes in a cerebrospinal fluid samples with a lower limit of detection of 10 pathogens in 1 ml of sample (100-fold improvement over existing assays).

[0014] In alternative embodiments of the invention, after the initial immunocapture and various wash steps, the cells may be lysed and the pathogen ATP and/or pyrophosphate (PPi) content determined, for example by BRC. In addition to its use for cell quantification, ATP levels indicate the metabolic state of the cell and may be assayed for a variety of applications. For example, BRC detection of ATP may be utilized to detect growth, or lack thereof, of bacteria in media containing antibiotics. Because very few cells are required for detection, BRC procedures can be used to detect growth of bacteria after only a few doubling-times, unlike present methods that require enough growth to result in a visible colony on a plate. In some embodiments, antibiotic sensitivity may be determined without identifying the pathogenic bacteria, for example by screening for bacterial growth in a variety of antibiotic solutions. Novel BRC procedures result in very rapid methods for determining the antibiotic resistance of a given bacterium.

[0015] In an alternative embodiment, resistance to lytic antibiotics may be monitored directly by simply detecting the intracellular ATP released into the solution following lysis by the antibiotics. Resistance of an organism to lysis would indicate antibiotic resistance of the organism. In this way BRC-enhanced detection can be used to measure the effects of antibiotic substances on microorganisms. Advantageously, very few cells are required for detection. Thus BRC procedures can be used to monitor antibiotic resistance of very few organisms, unlike present methods that require enough growth to result in a visible colony on a plate. Such detection methods eliminate the step of culturing microbial samples in microbial growth media altogether. Elimination of this culture step greatly speeds up the process of determining the antibiotic resistance properties of pathogens, and thus provides life-saving information in a timely fashion.

[0016] In other embodiments of the invention, the pathogen may be detected using oligonucleotide or nucleic acid tags attached to a protein or peptide, such as an antibody, that binds to the pathogen or to a pathogen molecule, such as a capsule or coat protein. The pathogen may be captured and/or isolated using known techniques, such as immunocapture, and the tag detected as disclosed below, for example by BRC assay. Detection may utilize a sandwich type assay, in which a first antibody binds to the pathogen and attaches it to a surface. Binding of a second, tagged antibody is followed by detection of the tag.

[0017] In some embodiments of the invention, pathogens may be detected by binding to an aptamer. Aptamers are oligonucleotides that exhibit specific binding interactions that are not based on standard Watson-Crick basepair formation. Aptamers are therefore similar to antibodies in their binding characteristics. Aptamers may be derived by an *in vitro* evolutionary process called SELEX (*e.g.*, Brody and Gold, *Molecular Biotechnology* 74:5-13, 2000). Aptamers are relatively small molecules on the order of 7 to 50 kDa that may be produced by known methods (*e.g.*, U.S. Patent Nos. U.S. Pat. Nos. 5,270,163; 5,567,588; 5,670,637; 5,696,249; 5,843,653) or obtained from commercial sources (*e.g.*, Somalogic, Boulder, CO). Because they are small, stable and not as easily damaged as proteins, they may be well suited for assays involving binding to the surface of a solid matrix. Because aptamers may be comprised of DNA, they can serve as substrates for terminal transferase or other enzymatic activity as disclosed below.

[0018] The captured and/or isolated targets may be detected, identified and/or quantified using a variety of enzymatic assays. Preferably, a product of the enzyme is detected by bioluminescence, for example by the BRC method discussed below. In certain embodiments of the invention, terminal transferase may be used to detect, identify and/or quantify pathogen nucleic acids. However, the skilled artisan will realize that a variety of enzyme based detection techniques may be utilized within the scope of the present invention, so long as the enzyme produces a product (*e.g.*, pyrophosphate, ATP, ADP, AMP, GTP, *etc.*) that can be assayed. Other enzymes that may be coupled to bioluminescent detection include DNA polymerases, RNA polymerases, reverse transcriptases, adenylate kinase, phosphoenolpyruvate kinase, and many other enzymes known in the art. In preferred embodiments of the invention, the enzyme coupled assay system produces pyrophosphate (PPi) and/or ATP. As discussed in more detail below, in more preferred embodiments bioluminescent detection may utilize a luciferin/luciferase coupled assay system, such as BRC.

[0019] In preferred embodiments of the invention, pathogen nucleic acids and/or oligonucleotide tags bound to pathogen specific antibodies may be detected, identified and/or quantified using a bioluminescence regenerative cycle (BRC) assay. The BRC process may be used to detect reaction products from a variety of enzymes. For example, terminal transferase may be added to a pathogen nucleic acid or oligonucleotide tag in the presence of nucleotides (dNTPs). Terminal transferase will add nucleotides to the 3' end of single-stranded DNA (ssDNA) or the 3' overhangs of double-stranded DNA that has been treated, for example, with a restriction endonuclease. Terminal transferase may also add nucleotides to blunt-ended double-stranded DNA or the recessed 3' ends of restricted double-stranded DNA, with lower efficiency. Incorporation of nucleotides by terminal transferase results in generation of pyrophosphate (PPi), with one molecule of PPi generated for each nucleotide incorporated. The skilled artisan will realize that the terminal transferase reaction is exemplary only and that many other enzymes, such as DNA or RNA polymerases, can also generate PPi by incorporation of nucleotides into DNA or RNA strands.

[0020] In certain embodiments of the invention, the pyrophosphate producing reaction is allowed to proceed to completion before BRC analysis. Once the reaction is complete, the pyrophosphate is reacted with APS (adenosine 5'-phosphosulfate) in the presence of ATP sulfurylase to produce ATP and sulphate. The ATP is reacted with oxygen and luciferin in the presence of luciferase to yield oxyluciferin, AMP and pyrophosphate. The PPi may react again with APS to regenerate ATP. For each molecule of pyrophosphate that is cycled through BRC, a photon of light is emitted with a quantum efficiency of 0.88 and one molecule of pyrophosphate is regenerated. Because of the relative kinetic rates of luciferase and ATP sulfurylase, a steady state is reached in which the concentrations of ATP and pyrophosphate and the level of photon output remain relatively constant over an extended period of time. The number of photons may be counted (integrated) over a time interval to determine the number of pathogen nucleic acids in the sample. Typically, each pathogen cell contains a single chromosome, providing a one-to-one correspondence between pathogen nucleic acids and pathogen cells.

[0021] The very high sensitivity of BRC is related in part to the integration of light output over time, in contrast to other methods that measure light output at a single time point or at a small number of fixed time points. The ability to vary the length of time over which photon integration occurs also contributes to the very high and controllable dynamic range for target

quantification, with a sensitivity of detection as low as 0.1 attomoles (amol). Increasing the length of integration also significantly reduces detection noise.

[0022] In preferred embodiments of the invention, steady state light output is subjected to data analysis involving integration of light output over a time interval, providing an accurate and highly sensitive method for quantifying the number of pathogens in the sample. In various embodiments of the invention, light output by BRC may be corrected for background light emission (for example, by PPi contaminating one or more reagents) by comparing enzyme (*e.g.*, terminal transferase) mediated photon emission with the background photon emission.

[0023] In other alternative embodiments of the invention, PPi generation may be assayed in real time as the PPi is produced. PPi may be reacted with APS to produce ATP, which can generate light via a luciferin/luciferase process as discussed above. Rather than reaching a steady state, light output may increase with time as an enzyme-coupled reaction produces an increasing concentration of PPi. The light output curve may be subjected to kinetic analysis to determine the amount of target cell or pathogen present in the sample. Such a process may exhibit increased sensitivity of detection by maximizing the amount of light output generated for a given amount of target cell or pathogen. In various embodiments the BRC assay may be modified to increase light output, for example by utilizing a super BRC assay, a branched BRC assay, a rolling circle BRC assay or a transcription based branched BRC assay as disclosed in more detail below.

[0024] In certain embodiments of the invention, thermostable enzymes may be used in a BRC or other detection method. Thermostable forms of terminal transferase, ATP sulfurylase and luciferase are disclosed herein and may be used for either isothermal processes or thermal cycling reactions. Thermostable forms of polymerases, such as *Taq* polymerase are known in the art and may be utilized in the disclosed methods.

[0025] In certain embodiments of this invention, to reduce the background signal of the assay caused by ATP and/or PPi contamination, ATP and PPi degrading enzymes, and or reagents may be used before the BRC procedure. After sufficient background reduction, the enzyme and/or reagent can be extracted or deactivated by physical or chemical means, resulting in a contamination free reaction solution for BRC assays. For instance apyrase (ATP-diphosphatase EC 3.6.1.5, Smartt *et. al.* 1995) can be used to degrade contaminating ATP, while pyrophosphatase (EC 3.6.1.1, Cooperman *et. al.* 1992) may be used to degrade

contaminating PPi molecules. Inactivation of these enzymes prior to BRC assay may be carried out by heating (e.g. 2 min above 80°C), which does not effect thermostable BRC enzymes.

[0026] The invention is not limited to use of ATP-Sulfurylase as the enzyme converting PPi to ATP. Other enzymes may be used to create the regenerative cycle as well (e.g., Heinonen, “Biological Role of Inorganic Pyrophosphate”, Kluwer Academic Publishers, 2001) if they are able to synthesis ATP out of PPi by consuming other substrates. Non-limiting examples of such enzymes are listed in Table 1 below.

TABLE 1. Exemplary ATP Producing Enzymes

Enzyme	Reaction	Reference
FMN Adenyltransferase [EC 2.7.7.2]	PPi + FAD ↔ ATP + FMN	Schrerer and Kornberg 1950
Adenylyl Transferase [EC 2.7.7.1]	PPi + NAD ⁺ ↔ ATP + nicotinamide ribonucleotide	Kornberg 1948
Glucose-1-Phosphate Adenyltransferase [EC 2.7.7.27]	PPi + ADP-glucose ↔ ATP + α-D-glucose-1-phosphate	Munch-Petersen <i>et al.</i> 1953

[0027] The invention is not limited to BRC assay of enzyme activity. It will be apparent to the skilled artisan that many different methods of assaying enzyme activity are known and may be used in the practice of the disclosed methods, such as incorporation of fluorescently tagged nucleotides and fluorescence spectroscopy; incorporation of radioactively tagged nucleotides and liquid scintillation counting or other radioassay; incorporation of Raman labels and Raman spectroscopy; incorporation of NMR labels and nuclear magnetic resonance assay, and many other techniques known in the art. In various embodiments of the invention, multi-color detection methods may be employed, using nucleotides tagged with different colored fluorophores.

[0028] In certain embodiments of the invention, the activity of the BRC process may be initially inhibited by the presence of a selected peptide covalently or non-covalently attached to one or more of the BRC enzymes, such as luciferase or ATP sulfurylase. Removal of the

inhibitory peptide by a protein or peptide present in a sample to be analyzed initiates the light emitting BRC reactions. In some embodiments the inhibitory peptide may be removed by a protease present in the pathogen. In other embodiments, the BRC enzymes may be activated by a protease attached to a pathogen specific antibody. The methods are not limited by the type of protease used, including but not limited to a serine protease, a cysteine protease, an aspartic protease, a metallo-protease, a cathepsin, a collagenase, an elastase, kallikrein, plasmin, renin, streptokinase, subtilisin, thermolysin, thrombin, urokinase, HIV protease, trypsin, chymotrypsin, pepsin, gastrin, calcium-dependent proteases, magnesium-dependent proteases, proteinase K, papain, bromelain, or any other protease known in the art. The specificities of various proteases for different target peptide sequences are well known in the art. In certain embodiments, the presence of a bacterial or viral encoded protease in a sample, such as HIV protease or streptokinase, may be diagnostic for the presence of an infection with a pathogenic organism.

[0029] Other embodiments of the invention concern compositions and/or apparatus of use for assaying cells or pathogens. In an exemplary embodiment, an apparatus of use may comprise one or more of the following components: reaction chambers for BRC or other enzymatic process and/or target cell or pathogen capture; microfluidic system to add reagents or extract products from the reaction chamber(s); magnetic capture devices; vibration generator and/or mixing apparatus; optical coupling means to convey photons to a photodetector; photodetectors; sensor arrays; cooling and/or heating apparatus to control reaction chamber, photodetector and/or sensor temperature; temperature control module and/or data acquisition and analysis system. In exemplary embodiments, a cooled CCD camera imaging system or luminometer may be used as optical detectors, although any other optical detector known in the art may be used. In embodiments where a photodetector with a single fixed aperture of limited field is employed, the apparatus may optionally comprise a stage and/or motion control system to move the photodetector relative to a series of samples, for example a 96 well microtiter plate or other sample holder. The embodiments of the invention are not limited to photodetection and any other type of detector known in the art may be utilized.

[0030] In other embodiments of the invention, the apparatus may comprise one or more monodirectional microfluidic flow components, such as a cassette containing channels and/or microchannels. The cassette may comprise one or more sealed chambers connected by a monodirectional flow, with each sealed chamber containing a specific affinity matrix to capture a target cell or pathogen. A sample may pass through the cassette and be exposed to

each chamber in turn, allowing binding of multiple target cells or pathogens to capture probes located in the chambers. After washing, the BRC detection reagents or other detection system reagents may be added and a signal, such as a bioluminescent signal, detected from each individual chamber. The chamber may be incorporated into a photodetection device or may be separately reacted with a sample and then inserted into a photodetection system. Many alternative forms of such a cassette system are known in the art and may be used, for example a microfluidic or capillary chip system as discussed in more detail below.

BRIEF DESCRIPTION OF THE DRAWINGS

[0031] The following drawings form part of the present specification and are included to further demonstrate certain aspects of the present invention. The invention may be better understood by reference to one or more of these drawings in combination with the detailed description of specific embodiments presented herein.

[0032] FIG. 1 illustrates exemplary methods using BRC to detect either the released pyrophosphate from nucleic acid polymerization or endogenous ATP in microorganisms. Nucleic acid polymerization results in the production of pyrophosphate, which is converted to ATP by ATP sulfurylase and APS. Alternatively, endogenous ATP may be measured after lysis of a cell or pathogen. The ATP is broken down to pyrophosphate and AMP by luciferin/luciferase with a resulting emission of visible light. The pyrophosphate is recycled to regenerate ATP, resulting in an increase in steady-state luminescence. In alternative embodiments of the invention, other pyrophosphate generating enzyme-mediated processes besides nucleic acid polymerization may be assayed by BRC. In other alternative embodiments of the invention, other enzymes besides ATP sulfurylase may be utilized to recycle PPi to ATP.

[0033] FIG. 2 shows a bioluminescence regenerative cycle block diagram of exemplary ATP sulfurylase and luciferase catalyzed reactions in BRC.

[0034] FIG. 3 shows a simulation of a comparison between luciferase generated light intensity in the presence and absence of ATP sulfurylase and APS at different starting concentrations of ATP (luciferin = 0.1 mM, APS = 0.1 mM), based on the kinetic properties of the enzymes.

[0035] FIG. 4 illustrates an exemplary method for branched chain BRC assay.

[0036] FIG. 5 illustrates an exemplary method for transcription based branched chain BRC assay.

[0037] FIG. 6 illustrates an exemplary method for bioluminescence super regenerative cycle (super BRC) assay.

[0038] FIG. 7. illustrates exemplary methods of terminal transferase based assays, involving capture and detection of a nucleic acid (1a-3a) or sandwich immunassay using a nucleic acid or oligonucleotide attached to an antibody, followed by extension of the 3' terminus using terminal transferase.

[0039] FIG. 8 illustrates a general method for detection and/or quantification of cells or pathogens, utilizing BRC assay of endogenous cell ATP and PPi.

[0040] FIG. 9 illustrates an exemplary apparatus for immunocapture and BRC assay, including a pathogen capture chip where a flow system directs the sample of interest through a plurality of chambers affinity matrices. Pathogen-specific binding moieties, such as antibodies or aptamers, are localized within each chamber to capture and enrich specific pathogens as they pass through the chamber. Following lysis and BRC assay, the detection of a signal from individual chambers indicates the presence of specific pathogens.

[0041] FIG. 10 illustrates a method and apparatus for BRC-enhanced ATP detection using a pathogen detection chip. (a) The sample is exposed to one or more affinity matrices containing binding moieties specific for different pathogens localized in different chambers. (b) The chambers are washed to remove unbound cells. (c) The cells are lysed and BRC detection reagents are added to the chambers. (d) The photon flux from each capture site is measured by an image sensor, such as a CCD detector or photomultiplier tube or array.

[0042] FIG. 11 shows an exemplary method for pathogen detection by using a pathogen specific amplification primer. An oligonucleotide primer specific to a particular pathogen DNA sequence is added to a complex sample containing various DNA molecules. This mix is allowed to hybridize with a capture oligonucleotide attached to a solid phase substrate. The unbound DNA is washed away and the appropriate polymerization mix is added, resulting in the release of pyrophosphate if the particular pathogen DNA is present in the test sample.

[0043] FIG. 12 illustrates an exemplary apparatus for use with BRC detection.

[0044] FIG. 13 shows an exemplary result of a BRC assay, comparing light emission from a 0.1 pmol sample with a reference standard.

[0045] FIG. 14 shows the increase in steady state light emission from a 10 fmol (femtomole) sample. Random noise in the light emission can be filtered out by detecting a steady-state change in the baseline level of light emission.

[0046] FIG. 15 Photon generation by BRC assay. Photon intensity (photon/sec) was measured using a CCD imaging system with a 96-well microtiter plate format. (a) The nucleic acid comprised 10 amol to 1 fmol of a 230 bp PCR product (Maltose binding protein). (b) The nucleic acid comprised a single-stranded 40bp oligo-loop, hybridized to itself, ranging in concentration from 1 fmol to 100 fmol. (c) The graph illustrates the quantitative results obtained, showing the dynamic range of the assay.

[0047] FIG. 16 Relative luminescence units measured by luminometer. Results normalized to a 1 fmol to 1 amol dilution series (incorporated dNTPs) for (a) ATP, (b) 40bp oligo-loop and (c) 230bp PCR product (Maltose binding protein).

[0048] FIG. 17 (a) Taqman results from three dilution series of 10 ng of *S. invicta* Queen GP-9B expression. (b) Relative luminescence units measured from 1 ng of the same pathogen nucleic acid with BRC.

[0049] FIG. 18 Relative luminescence from 40 µl of BRC reaction buffer using different dilutions of lysate from (a) U937 macrophage cells and (b) *E. coli*.

[0050] FIG. 19 shows an exemplary embodiment of BRC applied to SNP detection.

[0051] FIG. 20 shows an exemplary embodiment of BRC applied to pathogen detection.

[0052] FIG. 21 shows an exemplary embodiment of BRC using a rolling circle technique.

[0053] FIG. 22 illustrates the use of BRC to detect complex genomic DNA, with and without amplification of the nucleic acid sequence. Detection and quantification of a RO 52 sequence was demonstrated.

[0054] FIG. 23 illustrates exemplary hypothetical waveforms for each of the bases adenine (A), guanine (G), cytosine (C) and thymine (T) that would be detected during DNA sequencing.

[0055] FIG. 24 illustrates an exemplary hypothetical waveform generated for an exemplary DNA sequence TCTAGCTCAG (SEQ ID NO:6).

[0056] FIG. 25 illustrates a noise-corrupted aggregate waveform obtained from a uniformly asynchronous reaction of 10^5 molecules of DNA with the exemplary sequence TCTAGCTCAG (SEQ ID NO:6).

[0057] FIG. 26 illustrates a reconstructed waveform using the Wiener solution ($SNR_{perfect} = 40db$).

[0058] FIG. 27 illustrates a reconstructed waveform using the Wiener solution ($SNR_{perfect} = 35db$).

[0059] FIG. 28 illustrates a reconstructed waveform using the Wiener solution ($SNR_{perfect} = 30db$).

[0060] FIG. 29 illustrates a reconstructed waveform using the Wiener solution ($SNR_{perfect} = 40db$ and $N = 10^6$).

[0061] FIG. 30 shows an exemplary noise-corrupted aggregate waveform of 10^5 DNA molecules with Gaussian delay distribution.

[0062] FIG. 31 illustrates an exemplary reconstructed waveform using the Wiener solution when the delay distribution is Gaussian ($SNR_{perfect} = 40db$).

[0063] FIG. 32 illustrates a schematic diagram of a photodetector consisting of a photodiode and an integrator with output potential for both high and low illumination.

[0064] FIG. 33 shows an exemplary assay for pathogen detection using magnetic bead capture and BRC assay.

[0065] FIG. 34 illustrates an exemplary method for quantification of specific pathogen using antibody capture and binding to a solid surface.

DESCRIPTION OF ILLUSTRATIVE EMBODIMENTS

Definitions

[0066] Terms that are not otherwise defined herein are used in accordance with their plain and/ordinary meaning.

[0067] As used herein, "a" or "an" may mean one or more than one of an item.

[0068] As used herein, the terms "analyte", "cell", "pathogen" and "target" mean any macromolecular complex of interest for detection. Typically, such complexes will be

membrane bound, for example by a lipid bilayer membrane. Non-limiting examples of targets include a biowarfare agent, biohazardous agent, infectious agent, virus, bacterium, *Salmonella*, *Streptococcus*, *Legionella*, *E. coli*, *Giardia*, *Cryptosporidium*, *Rickettsia*, spore, mold, yeast, algae, amoebae, dinoflagellate, unicellular organism, pathogen or cell. In certain embodiments, cells exhibiting a particular characteristic or disease state, such as a cancer cell, may be targets. Non-limiting examples of target pathogens are provided in Table 2 below.

Table 2. Non-limiting Exemplary Pathogens

<i>Actinobacillus spp.</i>	<i>B. suis</i>
<i>Actinomyces spp.</i>	<i>Brugia spp.</i>
Adenovirus (types 1, 2, 3, 4, 5 et 7)	<i>Burkholderia mallei</i>
Adenovirus (types 40 and 41)	<i>Burkholderia pseudomallei</i>
<i>Aerococcus spp.</i>	<i>Campylobacter fetus subsp. fetus</i>
<i>Aeromonas hydrophila</i>	<i>Campylobacter jejuni</i>
<i>Ancylostoma duodenale</i>	<i>C. coli</i>
<i>Angiostrongylus cantonensis</i>	<i>C. fetus subsp. jejuni</i>
<i>Ascaris lumbricoides</i>	<i>Candida albicans</i>
<i>Ascaris spp.</i>	<i>Capnocytophaga spp.</i>
<i>Aspergillus spp.</i>	<i>Chlamydia psittaci</i>
<i>Bacillus anthracis</i>	<i>Chlamydia trachomatis</i>
<i>Bacillus cereus</i>	<i>Citrobacter spp.</i>
<i>Bacteroides spp.</i>	<i>Clonorchis sinensis</i>
<i>Balantidium coli</i>	<i>Clostridium botulinum</i>
<i>Bartonella bacilliformis</i>	<i>Clostridium difficile</i>
<i>Blastomyces dermatitidis</i>	<i>Clostridium perfringens</i>
Bluetongue virus	<i>Clostridium tetani</i>
<i>Bordetella bronchiseptica</i>	<i>Clostridium spp.</i>
<i>Bordetella pertussis</i>	<i>Coccidioides immitis</i>
<i>Borrelia burgdorferi</i>	Colorado tick fever virus
<i>Branhamella catarrhalis</i>	<i>Corynebacterium diphtheriae</i>
<i>Brucella spp.</i>	<i>Coxiella burnetii</i>
<i>B. abortus</i>	Coxsackievirus
<i>B. canis</i> ,	Creutzfeldt-Jakob agent, Kuru agent
<i>B. melitensis</i>	Crimean-Congo hemorrhagic fever

virus	Hepatitis B virus
<i>Cryptococcus neoformans</i>	Hepatitis C virus
<i>Cryptosporidium parvum</i>	Hepatitis D virus
Cytomegalovirus	Hepatitis E virus
Dengue virus (1, 2, 3, 4)	Herpes simplex virus
Diphtheroids	<i>Herpesvirus simiae</i>
Eastern (Western) equine encephalitis virus	<i>Histoplasma capsulatum</i>
Ebola virus	Human coronavirus
<i>Echinococcus granulosus</i>	Human immunodeficiency virus
<i>Echinococcus multilocularis</i>	Human papillomavirus
Echovirus	Human rotavirus
<i>Edwardsiella tarda</i>	Human T-lymphotrophic virus
<i>Entamoeba histolytica</i>	Influenza virus
<i>Enterobacter spp.</i>	Junin virus / Machupo virus
Enterovirus 70	<i>Klebsiella spp.</i>
<i>Epidermophyton floccosum</i> ,	Kyasanur Forest disease virus
<i>Microsporum spp. Trichophyton spp.</i>	<i>Lactobacillus spp.</i>
Epstein-Barr virus	<i>Legionella pneumophila</i>
<i>Escherichia coli</i> , enterohemorrhagic	<i>Leishmania spp.</i>
<i>Escherichia coli</i> , enteroinvasive	<i>Leptospira interrogans</i>
<i>Escherichia coli</i> , enteropathogenic	<i>Listeria monocytogenes</i>
<i>Escherichia coli</i> , enterotoxigenic	Lymphocytic choriomeningitis virus
<i>Fasciola hepatica</i>	Marburg virus
<i>Francisella tularensis</i>	Measles virus
<i>Fusobacterium spp.</i>	<i>Micrococcus spp.</i>
<i>Gemella haemolysans</i>	<i>Moraxella spp.</i>
<i>Giardia lamblia</i>	<i>Mycobacterium spp.</i>
<i>Giardia spp.</i>	<i>Mycobacterium tuberculosis, M. bovis</i>
<i>Haemophilus ducreyi</i>	<i>Mycoplasma hominis, M. orale, M. salivarium, M. fermentans</i>
<i>Haemophilus influenzae (group b)</i>	<i>Mycoplasma pneumoniae</i>
Hantavirus	<i>Naegleria fowleri</i>
Hepatitis A virus	<i>Necator americanus</i>

Neisseria gonorrhoeae
Neisseria meningitidis
Neisseria spp.
Nocardia spp.
 Norwalk virus
 Omsk hemorrhagic fever virus
Onchocerca volvulus
Opisthorchis spp.
Parvovirus B19
Pasteurella spp.
Peptococcus spp.
Peptostreptococcus spp.
Plesiomonas shigelloides
Powassan encephalitis virus
Proteus spp.
Pseudomonas spp.
 Rabies virus
 Respiratory syncytial virus
 Rhinovirus
Rickettsia akari
Rickettsia prowazekii, R. canada
Rickettsia rickettsii
 Ross river virus / O'Nyong-Nyong virus
 Rubella virus
Salmonella choleraesuis
Salmonella paratyphi
Salmonella typhi
Salmonella spp.
Schistosoma spp.
 Scrapie agent
Serratia spp.
Shigella spp.
 Sindbis virus

Sporothrix schenckii
 St. Louis encephalitis virus
 Murray Valley encephalitis virus
Staphylococcus aureus
Streptobacillus moniliformis
Streptococcus agalactiae
Streptococcus faecalis
Streptococcus pneumoniae
Streptococcus pyogenes
Streptococcus salivarius
Taenia saginata
Taenia solium
Toxocara canis, T. cati
Toxoplasma gondii
Treponema pallidum
Trichinella spp.
Trichomonas vaginalis
Trichuris trichiura
Trypanosoma brucei
Ureaplasma urealyticum
 Vaccinia virus
 Varicella-zoster virus
 Venezuelan equine encephalitis
 Vesicular stomatitis virus
Vibrio cholerae, serovar 01
Vibrio parahaemolyticus
Wuchereria bancrofti
 Yellow fever virus
Yersinia enterocolitica
Yersinia pseudotuberculosis
Yersinia pestis

BRC Detection

[0069] Various embodiments of the invention concern novel methods for quantifying target cells or pathogens without labeling of any target, capture or probe molecules. Such label free methods are advantageous with respect to sensitivity, expense and ease of use. In certain embodiments, the BRC methods involve the luminescent detection of pyrophosphate (PPi) molecules released from an enzyme-catalyzed reaction, such as RNA or DNA polymerization or terminal transferase catalyzed nucleotide addition. As part of the technique, a bioluminescence regenerative cycle (BRC) is triggered by the release of inorganic pyrophosphate (PPi).

[0070] Pyrophosphate based detection systems have been used for DNA sequencing (*e.g.*, Nyren and Lundin, *Anal. Biochem.* 151:504-509, 1985; U.S. Patent Nos. 4,971,903; 6,210,891; 6,258,568; 6,274,320, each incorporated herein by reference). The method uses a coupled reaction wherein pyrophosphate is generated by an enzyme-catalyzed process, such as nucleic acid polymerization. The pyrophosphate is used to produce ATP, in an ATP sulfurylase catalyzed reaction with adenosine 5'-phosphosulphate (APS). The ATP in turn is used for the production of light in a luciferin-luciferase coupled reaction. However, the "pyrosequencing" technique is based on sequential addition of single nucleotides, in the presence of nucleotide degrading enzymes to remove any unincorporated nucleotides (U.S. Patent Nos. 6,210,891 and 6,258,568). This results in low levels of light emission, with relatively low sensitivity, and requires a complex and expensive apparatus to perform the assay. The BRC method results in improved light emission and sensitivity of target detection.

[0071] The BRC cycle is illustrated in FIG. 1. Two alternative embodiments are presented in FIG. 1. The first involves the formation of PPi by some enzyme-mediated process, followed by reaction of PPi with APS to produce ATP and inorganic sulphate. The latter reaction is catalyzed by ATP-sulfurylase. Alternatively, endogenous ATP present in a cell or pathogen may be measured after lysis of the cell or pathogen. In either case, luciferin and luciferase consume ATP as an energy source to generate light, AMP and oxyluciferin and to regenerate PPi (FIG. 1). Thus, after each BRC cycle, a quantum of light is generated for each molecule of PPi (or endogenous ATP) originally present in solution, while the net concentration of ATP in solution remains relatively stable and is proportional to the initial concentration of PPi (or ATP). In the course of the reactions, APS and luciferin are consumed and AMP and oxyluciferin are

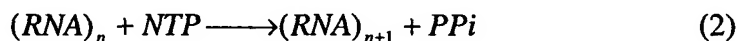
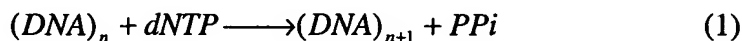
generated, while ATP sulfurylase and luciferase remain constant. The invention is not limited as to the type of luciferase used. Although certain disclosed embodiments utilized firefly luciferase, any luciferase known in the art may be used in the disclosed methods.

[0072] As illustrated in FIG. 1, where the enzyme mediated production of PPi is completed before initiation of bioluminescence, the photon emission rate remains steady and is a monotonic function of the amount of PPi in the initial mixture. For very low concentrations of PPi (10^{-8} M or less), the total number of photons generated in a fixed time interval is proportional to the number of PPi molecules. Where PPi is generated by the polymerase catalyzed replication of a pathogen nucleic acid, by terminal transferase mediated addition of nucleotides to the 3' end of a pathogen nucleic acid, or for any other enzyme mediated process where the amount of target cell or pathogen is a limiting factor, the number of photons generated in a fixed time interval is proportional to the quantity of the target cell or pathogen present in the sample. This is also true in alternative embodiments where endogenous ATP present in a cell or pathogen is assayed instead of PPi generated by nucleic acid polymerization.

[0073] The basic concept of enzymatic light generation from PPi molecules was introduced almost two decades ago (Nyren and Lundin, 1985; Nyren, *Anal. Biochem.* 167:235-238, 1987). Pyrophosphate based luminescence has been used for DNA sequencing (Ronaghi *et al.*, *Anal. Biochem.* 242:84-89, 1996) and SNP detection (Nyren *et al.*, *Anal. Biochem.* 244:367-373, 1997). The present methods provide additional procedures for accurately quantifying specific pathogen nucleic acids in low density arrays or other systems, in the presence of contaminants and detector noise. The novel system and methods have an intrinsic controllable dynamic range up to seven orders of magnitude and are sensitive enough to detect pathogen nucleic acids at attomole (10^{-18}) or lower levels. Other features of the "pyrosequencing" method disclosed by Nyren and others include addition of a single type of nucleotide at a time, either sequentially or to separate reaction chambers, and addition of nucleotide degrading enzymes such as apyrase to the pyrosequencing reaction (see, *e.g.*, U.S. Patent Nos. 6,210,891 and 6,258,568). Such processes are designed to measure bioluminescent light emission as single light pulses of limited intensity and duration. Advantages of the BRC process disclosed herein include the attainment of steady-state light emission, allowing data accumulation by integration of photon emission over time, and amplification of photon emission by recycling of PPi to regenerate ATP.

Analysis of Steady State BRC and Pyrophosphate-Based Assays

[0074] In various enzyme-catalyzed reactions, PPi molecules are generated when nucleotides (dNTPs or NTPs) are incorporated into a growing nucleic acid chain. For each addition of a nucleotide, one PPi molecule is cleaved from the dNTP by the enzyme (*e.g.* Klenow fragment of DNA polymerase I, RNA polymerase or terminal transferase) and released into the reaction buffer. The reactions catalyzed by DNA and RNA polymerases are shown in Eq. 1 and Eq. 2.



[0075] If one assumes that the strand is completely polymerized, then the number of PPi molecules (N_{PPi}) released during the process is given by Eq. 3.

$$N_{PPi} = N_{NA} \cdot (L_{NA} - L_P). \quad (3)$$

Where N_{NA} is the total number of primed nucleic acid molecules present in the reaction buffer, and L_{NA} and L_P are respectively the lengths of the nucleic acid chain and the primer.

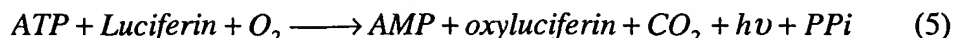
Enzymatic Bioluminescence Cycle

[0076] In preferred embodiments of the invention, photons may be generated from pyrophosphate by using ATP-sulfurylase (Ronesto *et al.*, *Arch. Biochem. Biophys.* 290:66-78, 1994; Beynon *et al. Biochemistry*, 40, 14509-14517, 2001) to catalyze the transfer of the adenylyl group from APS to PPi, producing ATP and inorganic sulfate (Eq. 4).



[0077] Next, luciferase catalyzes the slow consumption of ATP, luciferin and oxygen to generate a single photon ($\lambda_{max}=562nm$, Q.E. ≈ 0.88) per ATP molecule, regenerating a molecule of PPi

and producing AMP, CO₂ and oxyluciferin (Eq. 5). (Brovko *et al.*, *Biochem. (Moscow)* 59:195-201, 1994)



Because the luciferase reaction is significantly slower than the ATP-sulfurylase reaction, in the presence of sufficient amounts of the substrates APS and luciferin a steady state cycle should be maintained, in which the concentration of ATP and the resulting levels of light emission remain relatively constant for a considerable time.

[0078] This steady state cycle is indicated schematically in FIG. 2. Because the steady-state photon emission is proportional to the initial concentration of PPi, the presence of minute amounts of PPi produced by a polymerase or other reaction should result in a detectable shift in baseline luminescence, even in the presence of considerable amounts of noise. The number of photons generated over time by the BRC cycle can potentially be orders of magnitude higher than the initial number of PPi molecules, which makes the system extremely sensitive compared to prior art methods. The increased sensitivity is provided by having a time-dependent amplification of light emission for each molecule of PPi present at the start of the BRC cycle, coupled with the ability to integrate photon emission over any selected time interval.

Photon Generation Rate

[0079] The photon generation rate of the system may be determined from the kinetics and steady state characteristics of the ATP sulfurylase and luciferase (Ronesto *et al.*, 1994; Beynon *et al.*, 2001; Brovko *et al.*, 1994). In the presence of saturating concentrations of APS and luciferin, the ATP-sulfurylase reaction is orders of magnitude faster than the luciferase reaction. Thus, the rate of photon generation will be limited by the kinetics of luciferase rather than ATP-sulfurylase. A simplified equation expressing light intensity (*I*) in a unit volume for the BRC process is shown in Eq. 6.

$$I = \alpha \cdot \frac{d}{dt} \left(\frac{N_{ATP}}{V} \right) = \alpha \cdot \left(\frac{k_L}{V} \right) N_{ATP} \quad (6)$$

N_{ATP} is the number of ATP molecules in the solution, k_L is the turnover rate constant of luciferase, V is the volume of the solution, and α is the quantum efficiency of the

bioluminescence process. Note that equation 6 applies when either PPI is utilized to make ATP or when endogenous cell ATP is measured.

[0080] If ATP-sulfurylase was not present in the buffer, the light intensity would never reach a steady state and would simply decay as a function of time. In the presence of ATP-sulfurylase and APS, any decrease in the concentration of ATP will be compensated almost instantly by reaction of the generated PPI molecule with APS to regenerate ATP. This will cause the system to stay in a quasi-equilibrium state, where the concentrations of ATP and PPI remain relatively constant. At the same time, the luciferase reaction is constantly occurring and photons are emitted in a steady state fashion (FIG. 3). If the concentrations of APS and luciferin are high enough to assure saturation, then the steady state light intensity is given by Eq. 7.

$$I = \alpha \cdot \left(\frac{k_L}{V} \right) (N_{PPI})_0 \quad (7)$$

$(N_{PPI})_0$ is the initial number of PPI molecules generated from the polymerization or other process. Where endogenous ATP is measured, the initial number of ATP molecules present in the target cells may be substituted into the equation. Combining equations 3 and 7 gives Eq. 8.

$$I = \alpha \cdot \left(\frac{k_L}{V} \right) N_{NA} \cdot (L_{NA} - L_P) . \quad (8)$$

[0081] Equation 8 shows the proportionality between the generated light intensity and the initial number of nucleic acid molecules in a unit volume. If the number of photons detected is accumulated for a time interval T (integration time), the total number of photons generated (N_{ph}) from the whole volume is given by Eq. 9.

$$N_{ph} = \alpha \cdot k_L \cdot T \cdot N_{NA} \cdot (L_{NA} - L_P) . \quad (9)$$

[0082] According to Eq. 9, the number of photons received by the detector (*e.g.* CCD camera) depends on the integration time and the number of target cells or pathogens present in the solution. By controlling the integration time the sensitivity of the system can be increased to any

desired level limited by the saturation of the optical system. The dynamic range of the sensor system may therefore be proportionately enhanced.

Noise and Background Contamination

[0083] There are two phenomena that might potentially interfere with the performance and sensitivity of cell or pathogen detection. One is the possibility of PPI and/or ATP contamination from the chemicals included in the buffer solution. The other is the noise of the detector (*e.g.* thermal noise and/or shot noise in a photodiode system). The effects of ATP and PPI contamination on light emission may be modeled by modifying Eq. 8 to account for an initial existing number of PPI (and/or ATP) molecules C_{PPI} , resulting in Eq. 10.

$$I = \alpha \cdot \left(\frac{k_L}{V} \right) \cdot [N_{NA} \cdot (L_{NA} - L_p) + C_{PPI}]. \quad (10)$$

[0084] Although C_{PPI} is relatively low for common bioluminescence measurements (on the order of 0.1 to 10 femtomoles), it can be an order of magnitude higher than the target cell or pathogen concentration. It is also possible to have variation between experiments in the value of C_{PPI} of as much as 300%. To eliminate the effects of any possible contamination, the light intensity of the system is initially measured in the absence of any PPI generated from polymerization or endogenous cell ATP. This serves as an initial reference point for measuring the catalytically produced PPI and/or endogenous cell ATP. If the light intensity in the reference state is I_r , by combining equations 9 and 10 the value of N_{NA} may be calculated from Eq. 11.

$$N_{NA} = \left(\frac{V}{\alpha \cdot k_L} \right) \frac{I - I_r}{L_{NA} - L_p} \quad (11)$$

In terms of number of photons detected;

$$N_{NA} = \left(\frac{1}{\alpha \cdot k_L} \right) \frac{N_{ph} - N_{phr}}{T \cdot (L_{NA} - L_p)} \quad (12)$$

[0085] To account for the noise of the system, it is assumed that the total noise of the detector $n(t)$ is random and has a normal distribution $N(0, \sigma)$, with a mean of zero and a standard deviation of σ . Thus, the apparent light intensity in the presence of detector noise is given by Eq. 13.

$$I(t) = \alpha \cdot \left(\frac{k_L}{V} \right) N_{NA} \cdot (L_{NA} - L_p) + n(t), \quad (13)$$

[0086] Integrating Eq. 13 over a time interval T ,

$$N'_{NA} = \left(\frac{V}{\alpha \cdot k_L} \right) \frac{\int_T I(\tau) d\tau}{(L_{NA} - L_p) \cdot T} = \left(\frac{1}{\alpha \cdot k_L} \right) \frac{N_{ph} - N_{phr} + \int_T (n_1(\tau) - n_2(\tau)) d\tau}{(L_{NA} - L_p) \cdot T} \quad (14)$$

where $n_1(t)$ and $n_2(t)$ are the noise introduced by the detector in the actual experiment and reference respectively. $n_1(t)$ and $n_2(t)$ are uncorrelated but have the same normal distribution of $N(0, \sigma)$. N'_{NA} is the measured nucleic acid quantity. Equation 14 can be rewritten as

$$N'_{NA} = N_{NA} + n'(t), \quad (15)$$

where $n'(t)$ is a normal distribution defined as

$$N'_{NA} - N_{NA} = n'(t) \rightarrow N \left(0, \sqrt{\frac{2}{T}} \cdot \frac{V\sigma}{\alpha \cdot k_L (L_{NA} - L_p)} \right) \quad (16)$$

[0087] As shown in Eq. 16, the difference between the estimated and actual quantity of the pathogen nucleic acid (measurement error) has a normal distribution. The standard deviation of error is a function of chemistry (k_L of luciferase in the assay), noise of the detector, and integration time. To achieve a selected level of error tolerance, the required integration time for a given chemistry and specific level of detector noise may be calculated.

[0088] The above analysis provides a quantitative basis for determination of the number of pathogen nucleic acid (or other) molecules present in a sample, accounting for the presence of contaminants and noise in the system. The resulting method provides a highly sensitive and

accurate procedure for determining the number of target cells or pathogens in a given sample. These methods are broadly applicable for a variety of techniques in which quantitative detection of target cells or pathogens is desired.

BRC Amplification Methods (Enhanced BRC)

[0089] In various embodiments of the invention, non-steady state BRC methods may be utilized to increase the signal strength (e.g., amplitude of photon emission) detected from a given number of target cells or pathogens. Many alternative methods for amplifying the light emission signal detected by BRC may be utilized. Exemplary methods, discussed below, include branched chain BRC, transcription based BRC and super BRC.

Branched BRC Assay

[0090] Pyrophosphate generation is not limited to the extension of a primer on a pathogen nucleic acid and/or oligonucleotide tag. An alternative to increase the amount of nucleic acid polymerization, and hence increase the amount of pyrophosphate generated, is to extend off of the primer itself (FIG. 4). This requires use of a first primer (target specific primer) that is partially complementary in sequence to the pathogen nucleic acid and/or oligonucleotide tag and partially complementary in sequence to a second primer. The second primer (oligo-loop primer) is partially complementary in sequence to the first primer, and partially complementary in sequence to itself. The first primer is allowed to bind to the pathogen DNA. The second primer is allowed to hybridize to a different portion of the first primer. The second primer then hybridizes to itself. Upon addition of polymerase and nucleotides, the second primer essentially primes its own duplication (FIG. 4), generating pyrophosphate in the process. FIG. 4 also illustrates an exemplary embodiment wherein a capture probe is used to bind to the pathogen nucleic acid and attach it to a solid substrate.

[0091] This branching method can potentially generate thousands of pyrophosphate molecules per target cell or pathogen. The specificity of pyrophosphate generation is limited by the hybridization processes (capture probe, first primer and second primer), not the polymerization process. If the extendable bases in the branch complex (second primer) is equal to L_b , then the light intensity from the unit volume of the reaction buffer which contains N_p branch probes is

$$I = \alpha \cdot \left(\frac{k_L}{V} \right) \cdot N_p \cdot L_x \quad (17)$$

Potentially, the branched chain method may be more sensitive than known methods, such as PCR™ amplification of the target itself.

Transcription-Based Branched BRC Assays

[0092] An alternative embodiment of the invention, transcription-based branched BRC assay (FIG. 5), is similar to the branched BRC method disclosed above. It differs in that instead of utilizing a self-complementary second primer, it incorporates a recognition site (promoter sequence) for RNA polymerase into the target specific primer (FIG. 5). The RNA polymerase recognition (promoter) sequence results in the generation of RNA molecules through the incorporation of nucleotides by RNA polymerase and therefore a steady generation of PPi molecules (FIG. 5). The method is not limiting for the type of polymerase utilized and could incorporate either prokaryotic or eukaryotic promoter sequences, to be used with a prokaryotic or eukaryotic RNA polymerase, respectively. Promoter sequences are well known in the art, as discussed further below.

[0093] The kinetics of the PPi generation in this method is a function of pathogen nucleic acid (bound primer) quantity and may be detected by real-time monitoring of light by BRC. The photon generation rate in this system grows as a linear function of time and can be defined in a unit volume by:

$$I(t) = \left(\frac{\alpha \cdot k_L}{V} \right) \cdot k_i \cdot N_P \cdot t, \quad (18)$$

where k_i is the average turnover rate of the overall polymerization process on the probes and N_P is the total number of target molecules in the volume.

Bioluminescence Super Regenerative Cycle (BSRC) Assays

[0094] The two exemplary embodiments of the invention discussed above increase the sensitivity of BRC detection by generating pyrophosphate from replication of the primer sequence. A third exemplary embodiment, bioluminescence super regenerative cycle (BSRC, or "super BRC") results in signal amplification through the generation of 2 ATP molecules for every pyrophosphate by utilizing an additional enzyme-coupled process. In the exemplary embodiment disclosed in FIG. 6, the additional enzymes are adenylate kinase and pyruvate

kinase, with phosphoenolpyruvate added. However, the skilled artisan will realize that alternative combinations of enzymes and substrates could potentially be utilized to obtain the same result.

[0095] As shown in FIG. 6, the BRC enzymes are used to produce ATP from APS and PPi. The ATP may be reacted with AMP in the presence of adenylate kinase, producing two molecules of ADP. In this method an additional enzymatic complex is added to the standard BRC reaction: Adenylate Kinase (AK) in the presence of AMP substrate, and pyruvate kinase (PK) in the presence of phosphoenolpyruvate (PEP). The additional enzymes can create two ATP molecules from a single ATP by substrate cycling. Adenylate kinase catalyzes the transfer of a phosphate group from ATP to AMP, creating two molecules of ADP. Pyruvate kinase catalyzes the transfer of a phosphate group from PEP to ADP to form ATP, resulting in the creation of two molecules of ATP for every molecule of ATP previously present. This process would exponentially increase the concentration of ATP molecules in the reaction buffer. Since bioluminescence light activity of luciferase is proportional to the ATP concentration, the amount of light generated grows exponentially as a function of time. The rate of light generation growth depends on the kinetics of AK and PK and the concentration of their substrates.

[0096] The light intensity generated by the BSRC method, considering an exponential growth rate of k for the concentration of ATP molecules, is a function of time defined by

$$I = \alpha \cdot \left(\frac{k_L}{V} \right) \cdot N_{PPi} \cdot \exp(kt) \quad (19)$$

[0097] The super BRC assay generates more photons compared to the standard BRC protocol discussed above. However, quantifying the original concentration of PPi involves kinetic analysis, in contrast to data analysis with normal BRC which analyzes steady state light emission. It will be apparent that this method can also be used to measure endogenous ATP levels.

[0098] In the super BRC method one or more primers may be designed to have sequences specific to a pathogen nucleic acid of interest. The primers may be initially added into the solution where the pathogen nucleic acid is potentially present. If the target is present in the sample, the primer(s) anneals to the pathogen DNA, and the quantity of the primed pathogen DNA is equal to the number of original target cells or pathogens in the sample. If a polymerase

enzyme is then added with dNTPs, the primed pathogen DNA may be extended with incorporation of nucleotides by polymerization. A single PPi molecule is generated for each nucleotide incorporated. If the length of polymerization is known, the quantity of the target cell or pathogen can be quantified, and its concentration can be determined. The light intensity generated in this process is

$$I = \alpha \cdot \left(\frac{k_L}{V} \right) \cdot N_p \cdot L_x \quad (20)$$

where N_p is the number of target cells or pathogens in the solution and L_x is the extendable length of the pathogen nucleic acid and/or oligonucleotide probe.

Terminal Transferase Based Assays

[0099] Particular embodiments of the invention concern methods to detect, identify and/or quantify the presence of pathogen nucleic acids and/or other molecules linked to oligonucleotide tags, by means of terminal transferase activity. Sources of and general methods applicable to terminal transferase assays are known in the art (*e.g.*, Chang and Bollum, *CRC Crit. Rev. Biochem.*, 21, 27-52, 1986; Roychoudhury *et al.*, *Nucl. Acids Res.* 3, 101-116, 1976; Tu and Cohen, *Gene* 10, 177-183, 1980; Boule *et al.*, *J. Biol. Chem.* 276, 31388–31393, 2001).

[00100] A general approach that may be used involves the initial capture or isolation of one or more specific pathogen DNA molecules, or a target moiety containing DNA probes (*e.g.*, antibody molecules linked with an oligonucleotide) from the sample. Isolation can be carried out by various solid surface methods (*e.g.* capturing probe-coated magnetic beads), affinity matrices or electrophoretic processes. Once a pathogen DNA has been captured or isolated, terminal transferase is added in the presence of nucleotides (dNTPs). Terminal transferase catalyzes the addition of dNTPs to the 3' terminus of DNA. The enzyme works on single-stranded DNA (ssDNA), as well as the 3' overhangs of double-stranded DNA (dsDNA). Its activity therefore resembles a DNA polymerase that does not require a primer, avoiding the need for a separate primer hybridization procedure. Because the enzyme can be used with double-stranded DNA, it does not require the separate isolation of single-stranded DNA. A general scheme for methods of use of terminal transferase for target cell or pathogen detection and/or quantitation is illustrated in FIG.7.

[00101] As disclosed in FIG. 7, the pathogen nucleic acid can be free (1a-3a). Alternatively, an oligonucleotide tag may be attached to another molecule, such as an antibody (1b-3b). In cases where the pathogen nucleic acid is an RNA molecule, such as a retroviral nucleic acid, the RNA may be converted to cDNA using reverse transcriptase, according to known protocols (*e.g.*, Berger and Kimmel, 1987; Molecular Sambrook *et al.*, 1989). The pathogen nucleic acid may be captured, for example, by hybridization to a sequence specific capture probe (2a). Alternatively, oligonucleotide tags attached to another molecule may be captured by a variety of known immobilization methods, such as sandwich immunoassay (2b). Once captured, the substrate may be washed to remove unbound nucleic acids and the bound target may be extended using terminal transferase (3a, 3b). Where capture oligonucleotides are used, the 3' end may be blocked, for example using dideoxy nucleotides, to prevent the terminal transferase from extending unhybridized capture probes.

[00102] The rate of terminal transferase mediated dNTP incorporation into the captured strand depends on the concentration of the enzyme, nucleotides and the relative amount of captured 3' termini (which is in turn a function of the amount of pathogen nucleic acid in the sample). Given the accurate determination of terminal transferase activity in a fixed time interval, and the initial nucleotide and enzyme concentrations, it is possible to correlate the measured terminal transferase activity with the concentration of pathogen nucleic acid (total amount of 3' terminus) in the sample.

[00103] Terminal transferase based assays measure the number of 3' termini of DNA molecules in the sample, independent of the DNA being the actual target or just a reporter species linked to a secondary target. The enzyme can in theory incorporate unlimited number of nucleotides into the strand. However in a fixed time interval, depending on the activity of the enzyme, this number will be within a given deterministic range. A typical terminal transferase reaction may be performed, for example, at 20°C in buffer containing 20 mM Tris acetate (pH 7.9) and 50 mM potassium acetate, supplemented with 1.5 mM CoCl₂. Alternative assay conditions include 50 mM potassium acetate, 20 mM Tris-acetate (pH 7.9), 10 mM magnesium acetate and 1 mM dithiothreitol, at 37°C. Additional conditions suitable for assay of terminal transferase activity are known (see, *e.g.*, Chang and Bollum, 1986; Roychoudhury *et al.*, 1976; Tu and Cohen, 1980; Boule *et al.*, 2001).

[00104] Although a preferred substrate for terminal transferase is protruding 3' ends, it will also less efficiently add nucleotides to blunt and 3'-recessed ends of ssDNA or dsDNA fragments. Cobalt is the necessary cofactor for activity of this enzyme. Terminal transferase may be purchased commercially (*e.g.*, Fermentas, Inc., Hanover, MD; Promega, Madison, WI; Stratagene, La Jolla, CA) and is usually produced by expression of the bovine gene in *E. coli*.

[00105] The growth of a DNA strand in a terminal transferase based assay can potentially result in a variety of detectable phenomena. Exemplary measurable changes produced by enzyme activity include, but are not limited to, intrinsic characteristics of the growing molecule itself (*e.g.*, molecular mass, overall charge) as well as natural products of the incorporation reaction (*e.g.* PPi). Alternatively other effects can be measured using extrinsic modifications. These may include various labels or fluorogenic species attached to or incorporated into the nucleotide substrates. In preferred embodiments, the BRC assay system is used to detect PPi generated by terminal transferase activity.

Immuno-BRC Assays

[00106] In various embodiments of the invention, BRC assay methods may be utilized in combination with immunoassay techniques, to provide for highly sensitive and selective detection, identification and/or quantification of pathogens. Antibodies against pathogen proteins may be commercially available or may be prepared as disclosed below. Antibody-based BRC assays are not limited to protein detection, but may be used to detect any cell or pathogen molecule or macromolecular complex against which an antibody may be prepared.

[00107] In one exemplary embodiment of the invention, based on a sandwich ELISA type detection method, a primary antibody against a target cell or pathogen of interest may be attached to a surface. A sample suspected of containing the target cell or pathogen may be exposed to the surface to allow binding of the target to the primary antibody. After washing, a secondary antibody that binds to a different epitope (or different molecule) of the same target cell or pathogen may be added. In various embodiments, the secondary antibody may be tagged with one or more oligonucleotides. In preferred embodiments, the secondary antibody may be labeled with a dextran molecule. Multiple oligonucleotide tags may be attached to dextran, allowing amplification of the BRC signal.

[00108] Dextran may be conjugated to antibodies by methods known in the art. For example, dextran-biotin conjugates may be purchased (*e.g.*, Molecular Probes, Inc.) and attached to an avidin or streptavidin labeled antibody. Oligonucleotide tags may be prepared incorporating reactive groups for attachment to dextran, or may be purchased from commercial sources (*e.g.*, amine-oligos, SH-oligos, acrydite-oligos or biotin-oligos from Integrated DNA Technologies, Coralville, IA). Methods for attachment of oligonucleotides to dextran may utilize published protocols (*e.g.*, Gingeras *et al.*, *Nucleic Acids Res.* 15:5373-90, 1987).

[00109] Tag oligonucleotides and/or nucleic acids bound to dextran may be used to detect secondary antibody binding to target cells or pathogens using any of the BRC techniques disclosed above, such as regular BRC, branched-chain BRC, transcription based BRC or super BRC. Alternatively, a terminal transferase-based BRC method may be used to detect, identify and/or quantify target cells or pathogens by immuno-BRC. In some embodiments of the invention, a self-priming oligonucleotide that hybridizes to itself may be used to initiate DNA polymerization and PPi generation for assay by BRC.

[00110] In alternative embodiments of the invention, luciferase may be attached to a primary or secondary antibody. Various immunoassay techniques, for example sandwich ELISA, may be performed to detect a target pathogen. After binding and washing, reagents comprising ATP, APS, ATP sulfurylase and luciferin may be added to initiate bioluminescent detection.

[00111] The skilled artisan will realize that many variations on immuno-BRC methods may be utilized within the scope of the claimed methods. For example, in alternative embodiments a primary antibody may be directly labeled with tag oligonucleotides attached to dextran. Samples suspected of containing target cells or pathogens may be cross-linked to a solid surface and the primary antibody allowed to bind to the target for detection by BRC assay. In other alternatives, target cells or pathogens may be immobilized on a surface and reacted with an unlabeled primary antibody. A secondary antibody labeled with tag oligonucleotides attached to dextran may bind to the first antibody and be detected by BRC. The latter method offers the advantage that a single type of tagged secondary antibody (*e.g.*, goat anti-mouse antibody) may be used to detect binding of a variety of primary antibodies.

[00112] In immuno-BRC assays where the tagged (secondary) antibody exhibits specific binding to a target cell or pathogen, a given sample may be assayed for a number of different

target cells or pathogens either simultaneously or sequentially. For example, an antibody array may be prepared on a protein chip using standard methods. After exposure of a sample to the array, a mixture of secondary antibodies of differing specificities may be added to the chip. The presence of a target cell or pathogen is indicated by a signal (*e.g.*, a bioluminescent signal) detected from a specific location on the chip. Using a sandwich immunoassay, detection of a target cell or pathogen on such a protein chip depends on the specificity of binding of both primary and secondary antibodies to the pathogen. In other alternative embodiments, specificity of detection may depend upon the particular oligonucleotide tag attached to an antibody. A mixture of antibodies could be labeled each with a distinct oligonucleotide tag sequence. Upon binding of tagged antibodies to one or more target cells or pathogens, primers designed to hybridize to a single oligonucleotide tag sequence may be added sequentially, followed by addition of polymerase, nucleotides and BRC assay reagents. After generation of a signal, the tagged molecules could be washed, a new primer specific for a different oligonucleotide tag could be added and BRC detection performed again.

[00113] The skilled artisan will realize that many variations on known immunoassay techniques may be performed with BRC or other detection methods, and any such known immunoassay protocol may be utilized in the disclosed methods.

Detection Pathogens Using Endogenous ATP and BRC

[00114] Generally speaking, microorganisms and other cells have a regulated number of ATP molecules that is typically a function of the species and the size of the cell or microorganism. Under certain conditions, the ATP content may also reflect the metabolic state of the cell and may be used, for example, to assay the effects of antibiotics or other agents on cells or pathogens. Where the target cells are cancer cells, for example, one may screen a variety of potential anti-cancer agents and utilize ATP content to provide a rapid, sensitive and inexpensive method of determining their efficacy against a given type of cancer, as indicated by a decrease in ATP content. Such methods would avoid the use of radioactively tagged nucleotides to monitor DNA replication in the cell.

[00115] Under normal conditions, a given type of cell and/or pathogen should contain relatively constant levels of ATP. To count the number of cells or microorganisms within a sample, one can lyse them and release the intracellular debris in the medium (for example by

centrifugation, filtration, sonication, heating, detergent lysis, organic phase extraction or other known techniques). Cell lysis methods are well known in the art and may utilize, for example, digestion with proteinase K and detergent solubilization with low concentrations of sodium dodecyl sulfate (SDS). The total concentration of ATP may then be determined by BRC assay. The light intensity emitted during the BRC assay is related to the concentration of enzymatic substrate (ATP and PPi) and consequently to the number of cells present in a sample. Total cell ATP and PPi content may be determined for various cell types to generate an average amount of ATP and PPi present in the individual cells, which may be used to quantify the number of cells in a sample. The general scheme involved determination of cell number in a sample is illustrated in FIG. 8.

[00116] In certain embodiments of the invention, the procedures for pathogen identification can be combined into a single protocol to function in a portable detection device. The device can comprise a portable, ultra-sensitive pathogen detection system that can identify known pathogens, classes of pathogens (e.g. gram-positive, gram-negative or mycoplasma bacteria, fungal organisms and viral organisms), and the antibiotic resistance profile of the detected microbial pathogens. Exemplary pathogens may include *E. coli*, *Pseudomonas aeruginosa* or any pathogens on the NIAID priority list. Antibodies to *E. coli* and *Pseudomonas aeruginosa*, as well as other organisms, are commercially available (e.g., Novus Biologicals and United States Biological). The procedures disclosed below for immunocapture and bioluminescence may be performed according to published protocols (e.g., Squirrell *et al.*, 2002; Peng *et al.*, *Journal of Microbiological Methods* 49:335-338, 2002).

[00117] In exemplary embodiments of the invention involving human pathogen profiling tests, one or more pathogen specific antibodies may be used to capture the target. Immunoaffinity methods suitable for target separation are known in the art, including but not limited to use of antibody-conjugated magnetic beads, attachment to glass or plastic beads and FACS (fluorescent activated cell sorter) attachment of antibodies to solid supports such as nitrocellulose or nylon membranes, or use of various affinity matrices (FIG. 33 and FIG. 34). Alternatively, the total number of cells or microorganisms in a given sample may be determined, in which case separation of specific targets is not necessary.

Sample Isolation

[00118] In various embodiments of the invention, samples suspected of containing one or more microorganisms and/or cells may be collected and processed. Sample processing may be used, for example, to remove contaminants that could interfere with pathogen detection by light quenching, enzyme inhibition, *etc.* The embodiments are not limiting as to the type of sample that may be analyzed, and samples may include without being limited to blood, serum, plasma, cerebrospinal fluid, lymphatic fluid, urine, stool, semen, lacrimal fluid, saliva, sputum, a biopsy sample, a tissue scraping, a swab sample, an endoscopic sample, a cell sample, a tissue sample, food, water, environmental swab samples, air samples and any other sample that could potentially contain cells and/or microorganisms. Samples may be initially processed using any of a variety of known procedures, such as homogenization, extraction, enzymatic digestion (*e.g.*, protease, nuclease), filtration, organic phase extraction, centrifugation, ultracentrifugation, column chromatography, HPLC, FPLC, electrophoresis or any other type of known sample preparation, without limitation. In various applications, it may be appropriate to separate a sample into specific components, such as separating a blood sample into a cellular component and a serum component. In preferred embodiments, the final prepared sample to be analyzed will comprise an aqueous preparation with possible known or unknown cells and/or microorganisms

Pathogen Detection by BRC Assay

[00119] The BRC assay is used to quantify the sample concentration of target cells and/or microorganisms. Quantitative analysis relies upon the relationship between the number of cells and/or microorganisms in a sample and the light intensity detected by the assay. Assuming that there are a regulated and fixed number of ATP molecules, N_{ATP} , and PPi, N_{PPi} , in each cell then the total number of detectable substrate molecules for BRC assay per cell, N_{Cell} is

$$N_{Cell} = N_{ATP} + N_{PPi} \quad (21)$$

[00120] Since the photon generation process of BRC is only a function of the turnover of luciferase, rather than ATP-sulfurylase, the simplified equation expressing light intensity I , is

$$I = \alpha \cdot \frac{d}{dt} \left(\frac{N_{ATP}}{V} \right) = \left(\frac{\alpha \cdot k_L}{V} \right) \cdot N_{Sub}(t), \quad (22)$$

or

$$I = \left(\frac{\alpha \cdot k_L}{V} \right) \cdot (N_{Sub})_0. \quad (23)$$

where V is the volume of the reaction buffer, k_L the turnover rate of luciferase, α the quantum efficiency of the bioluminescence process, and $(N_{Sub})_0$ the initial quantity of BRC substrates (PPi and ATP) in the reaction buffer volume. With X number of cells in the sample, the light intensity based on (21) and (23) is

$$I = \left(\frac{\alpha \cdot k_L}{V} \right) \cdot X \cdot N_{Cell}, \quad (24)$$

[00121] Thus, the light intensity out of the assay is in fact proportional to the cell count. As an example if there are 10^6 substrate molecules per cell, then in order to assess the cell count from an assay, emitting I_x photons per second per unit volume, the following relationship would apply.

$$N_{Cell} = \frac{I_x}{\left(\frac{\alpha \cdot k_L}{V} \right) \cdot X} = \frac{I_x}{\left(\frac{\alpha \cdot k_L}{V} \right) \cdot 10^6}, \quad (25)$$

As disclosed herein, the BRC assay may be used to accurately quantify the number of target cells and/or microorganisms present in a sample, based on the emitted light intensity. Accurate estimates of cell and/or microorganisms number will be based on estimates of the amount of ATP and PPi per cell or microorganism. As the skilled artisan will appreciate, a variety of methods are available to derive such estimates. For example, target cells and/or microorganisms may be isolated from a given sample and the number of cells counted by a variety of known techniques, such as cell sorting by FACS, microscopic estimates of cell number, *etc.* The sample, containing a known number of cells, may then be subjected to BRC assay and the light

emission quantified. Using such techniques, the number of cells and/or microorganisms in a new sample may be determined simply based on the relationship of BRC emitted light per unit cell, without separately quantifying ATP and PPi. Alternatively, the ATP and PPi content per cell or microorganism may be determined by chemical analysis or may be obtained from reported values in the literature. The light emission from BRC may be quantified using known amounts of ATP and/or PPi standard solutions. Light emission from a new sample may then be related to ATP plus PPi content and the cells quantified.

Pathogen Detection With BRC Amplification

[00122] Various embodiments of the invention concern the use of BRC amplification methods for ATP detection. Exemplary BRC amplification methods include, but are not limited to, branched BRC, transcription-based branched BRC and super BRC, as discussed above. In certain embodiments, BRC amplification may be used to determine the total number of cells or microorganisms present in a sample. Preferably, pathogens are detected in a clear solution containing little or no contaminants. General methods for pathogen processing may utilize known procedures (*e.g.*, Squirrell *et al.*, 2002), with detection by BRC assay. In assays to detect pathogens in general, without identification of specific bacterial types, super BRC may be used to detect the presence of ATP that is normally found in bacterial cells. The super BRC assay does not require either probes or primers and is therefore independent of the pathogen nucleic acid sequence. The process is very sensitive and rapid, taking only a few minutes to obtain a signal. While the general assay does not identify the type of bacteria that are the source of ATP, it can rapidly determine if bacteria are present in a given sample.

[00123] Prior to BRC analysis, any bacteria present are lysed using known methods, such as sonication and freeze-thaw methods. Super BRC assay reagents are then added to the sample, including ATP sulfurylase, firefly luciferase, adenylate kinase and pyruvate kinase. If lysed bacteria are present in the sample, the ATP will be released and light will be generated with the addition of the appropriate reagents. In certain embodiments of the invention, thermostable forms of the enzymes may be utilized to allow BRC assay at higher temperatures.

[00124] In a regular BRC assay, the sensitivity for ATP detection is about 10^{-16} moles of ATP. With super BRC, about 10^{-18} moles of ATP can be detected, a 100-fold improvement in sensitivity. Because of the increased sensitivity of BRC amplification methods, it is envisioned

that concentration of organisms by binding to specific capture antibodies will allow detection of a single organism without requiring culture or growth of the organism. This will enable very rapid detection and specific identification, as discussed below.

Antibody-Based Pathogen Identification

[00125] Certain embodiments of the invention concern methods and apparatus for pathogen detection using immunocapture of organisms and BRC detection of ATP. Various cells and pathogens have unique surface antigens to which specific antibodies, aptamers or other binding moieties can attach. Pathogen specific antibodies are commercially available from a variety of companies (*e.g.*, Novus Biologicals and United States Biological), or may be prepared using known methods. Immunocapture methods may utilize known protocols for pathogen binding (*e.g.*, Peng *et al.*, *Journal of Microbiological Methods*, 49:335-338, 2002).

[00126] In particular embodiments of the invention, an apparatus as illustrated in FIG. 9 may be utilized for immunocapture and BRC assay. A flow channel connects one or more chambers within a chip, each chamber containing one or more capture moieties (*e.g.*, antibodies) specific or selective for a particular type of pathogen. In the illustrative example shown in FIG. 9, the four chambers contain antibodies for gram positive and gram negative bacteria, fungi and tuberculosis bacillum. Sample is injected through an inlet port and flows through each chamber sequentially, exiting through an outlet port. As sample passes through each chamber, pathogens that are recognized by the binding moieties in that chamber will bind and be immobilized. Non-specific pathogens will pass through the chamber and be washed out. Immobilized pathogens may be lysed and their ATP content determined by BRC assay. Secondary inlets associated with each chamber may be utilized for introduction of BRC reagents.

[00127] As shown in FIG. 9, the chambers may be covered by a light transparent covering, allowing the BRC or other photodetection assays to be performed on the chip. A CCD camera, photodiode or any other photodetector known in the art may be closely opposed to the chip, or optical fibers or other light conducting elements may conduct light from the individual chambers to a photodetector. In various embodiments of the invention, the chip and/or photodetector may be thermally regulated, for example to allow isothermal or cyclic thermal reactions to take place or to increase the efficiency of photodetection. In preferred embodiments of the invention, the chips may be designed to be inserted into a system or apparatus comprising a photodetector,

thermal regulator, pumps, valves, and any other accessory devices. The chips may be interchangeable and may be preloaded with antibodies or other capture moieties targeted against specific groups of pathogens. Different chips may be preloaded with binding moieties to detect standard pathogens present in urinary tract infections, blood infections, cerebrospinal fluid infections, lung infections, *etc.* Specialized chips may be designed to detect pathogens in biowarfare samples, water samples, air samples or other environmental samples. Alternatively, instead of an apparatus or system with exchangeable chips, a portable sensor device may be designed with a fully integrated, non-exchangeable chip. Different sensors may contain different antibodies or other binding moieties, depending on the type of samples to be processed. Systems designed with interchangeable chips are preferred in order to maximize the flexibility of the system for detection of different pathogens. Binding moieties with limited storage life may also be utilized more efficiently with an interchangeable chip system. Chips may be provided with preloaded antibodies or other binding moieties, or blank chips may be provided for loading with particular antibodies of interest to the individual user.

[00128] Binding moieties may be localized in individual chambers using any immobilization technique known in the art. For example, a capture membrane such as biotinylated nitrocellulose may be used as one surface of the chambers. Specific antibodies may be attached via covalent linkage to streptavidin or avidin, with different antibodies introduced into specific chambers. In alternative embodiments, antibodies may be attached to a membrane or other substrate using covalent cross-linking or other immobilization techniques as discussed below. Antibodies and other binding moieties may be attached to the substrate within the chamber, or may be attached to the substrate outside the chip with subsequent insertion of the substrate into the chip. Other methods of attachment of antibodies, aptamers, lectins or other binding moieties include use of nickel chelates bound to the polyhistidine regions of proteins, and other means of attachment well known in the art. Such alternative attachment procedures can be found in standard references, for example “The Handbook of Fluorescent Probes and Research Chemicals,” (Molecular Probes, Inc., Eugene, OR), which is incorporated herein by reference.

[00129] In particular embodiments of the invention, the binding moieties may be chemically attached to a hydrogel, such as a polyacrylamide based hydrogel (*e.g.*, Yu *et al.*, BioTechniques 34:1008-1022, 2003. Acrylamide monomers may be copolymerized with different probes (*e.g.*, oligonucleotides, DNA, proteins, aptamers, *etc.*) by photoinduced polymerization of methacrylic

modified monomers. Binding moieties may be localized in different chambers as discussed above. The hydrogels may be attached to glass, silicone or other surfaces. Avidin-modified binding moieties may be attached to hydrogels containing biotin-modified monomers. The use of hydrogels improves the stability of binding moieties, such as proteins, and can maintain their binding activity for six months or longer (Yu *et al.*, 2003). Hydrogel based chips may be utilized in combination with optical detection methods, such as BRC.

[00130] The binding moieties may be attached to the surface of the gel or alternatively may be embedded within the hydrogel to increase their stability. Where the binding moieties are embedded within the hydrogel, assays for the presence or absence of target molecules may also be performed within the gel. The hydrogel may be used to confine the reaction and/or enzymes, making localized BRC possible. Such assays may be performed using, for example, nucleic acid detection or immunoassay. The target and assay method are not limiting and virtually any target that can permeate into the hydrogel may be assayed by the disclosed method. Such localized assays allow for the possibility that more than one binding moiety-target interaction could be assayed within the same hydrogel.

[00131] Antibodies, lectins, or other means for specifically binding pathogens may be used to immobilize intact microorganisms in the flowing sample stream. The flow may be maintained by “wicking” of the aqueous sample fluid through a hydrophilic membrane, such as nitrocellulose or the like, into a high-capacity absorbent reservoir (filled with absorbent hydrophilic membrane) at the end of the channel. Alternatively, fluid flow may be maintained by external pumps, pistons, electroosmosis, pressure gradients or any other known means. The invention is not limited as to the surface for attachment of binding moieties and in alternative embodiments the chambers may be filled with magnetic beads linked to specific capture antibodies. The beads can be localized to desired detection region by using a fixed or electromagnet at the specific detection regions.

[00132] Samples may comprise phosphate-buffered saline (PBS) samples, blood, urine, throat swab, vaginal swab, cerebrospinal fluid, or other clinical, veterinary, air or water samples. The samples may contain various dilutions of microbes or pathogens. Antibodies or other binding moieties specific to the microbes or pathogens of interest to be detected may be bound to the surfaces of the capture membrane. Small amounts of samples to be tested may be placed on the membrane by means of a channel with a small external opening for introduction of the sample.

Alternatively a sample well may be used to house the membrane and sample. If a microbe of interest is present in the sample, it will bind to the specific antibody on the membrane. In some embodiments, capture of the organism may be verified by binding of a fluorescent-labeled second antibody. Once a sufficient binding time (e.g., 15 minutes) has elapsed, the surface is washed and unbound antibodies are removed. The relative intensity of fluorescence label (compared to a fluorescence standard) indicates the number of organisms that have been captured. The predetermined specificity of the antibody, or other selected specific ligand, allows the species of organism detected to be identified.

[00133] Alternatively, reagents for BRC-amplified detection of ATP may be introduced into the chamber. The organisms may be lysed, *in situ*, by standard heating, sonication, solvent, or detergent-lysis protocols. If a pathogen of interest is present at any specific capture site, that site will emit luminescence from the luciferase reaction. As shown in FIG. 10, the luminescence from the specific antibody capture sites may be imaged onto an electronic imaging device such as a charge-coupled device (CCD) detector, photodiode array, photomultiplier tube array, or the like. Commercially available imaging software, such as that available from Universal Imaging Corp. can be utilized to map the luminescence emission sites to specific antibody capture sites and indicate the identity of the pathogen(s) present in a sample. Alternatively, single point photodetectors, such as single photodiodes or photomultiplier tubes may be used for detection of emitted luminescence. Imaging software may be customized for specific applications using techniques readily performed by those skilled in the art

[00134] In some embodiments of the invention, BRC-enhanced luminescence detection of ATP (or PPi) causes the luciferase reaction to proceed at the maximum possible rate for a constant (steady-state) concentration of ATP (with no depletion of ATP) because ATP is regenerated by the BRC recycling reaction.

[00135] In a preferred embodiment of the invention, lysis of the captured microorganism is performed by heating to 90°C for 1-5 minutes. The luciferase and ATP sulfurylase to be used for this assay are thermally stable (less than 10% of the enzyme activity is lost during this heating protocol). Each organism detected may be sonicated for increasing periods of time (10, 20, 60 seconds) in order to determine if maximal lysis and release of ATP is achieved by heating alone. The BRC-enhanced ATP detection procedure has the advantage of being about 100 times more

sensitive than traditional ATP detection assays. This procedure enables the detection of pathogens at a much lower abundance level, thereby reducing the need for time-consuming culture of organisms to provide the minimum detectable number of organisms.

Nucleic Acid Based Pathogen Detection

Specific Pathogen Identification

[00136] Microbial capture and BRC-enhanced ATP detection can be combined with nucleic acid-based identification methods to increase the specificity of the overall identification. In nucleic acid-based identification assays, luminescence may be generated at specific DNA or RNA capture probe sites following DNA polymerase-catalyzed extension of nucleic acid primers. The extension reaction results in consumption of dNTP substrate molecules and the release of pyrophosphate (PPi) product molecules. Alternatively, terminal transferase or other pyrophosphate generating enzymes may be used. The PPi is detected by BRC assay, as described above.

[00137] An exemplary embodiment is illustrated in FIG. 11. Microorganism nucleic acids may be hybridized to capture probes immobilized on specific capture sites placed downstream of microbial immunocapture sites, after lysis and release of nucleic acids. The combination of immunocapture of pathogens with pathogen specific nucleic acid capture and amplification provides three levels of specificity, dependent on pathogen specific antibody binding, capture probe binding and primer binding. In alternative embodiments of the invention, pathogen nucleic acids may be detected without initial immunocapture.

[00138] In either case, one or more specific amplification primers may be added (FIG. 11). In different embodiments, either a single pathogen-specific primer may be utilized at a time, or else a mixture of primers specific to different pathogens may be added simultaneously, for example using a flow-through system. In embodiments utilizing an apparatus as illustrated in FIG. 9 and FIG. 10, with secondary inlets for each chamber, different primers specific for a particular pathogen nucleic acid sequence may be simultaneously added to different chambers. The primers bind to the immobilized nucleic acids and are thus localized to the specific capture probe sites. The primers may be extended by DNA polymerase to yield pyrophosphate. Any type of BRC assay disclosed herein may be utilized to detect the PPi. The pyrophosphate recycling

feature of the BRC reaction results in about a 100-fold increase in sensitivity for detection of pyrophosphate.

[00139] In such a system, the specificity of pyrophosphate generation is created by immunocapture, hybridization fidelity and the high degree of enzymatic specificity and polymerization accuracy. The sensitivity of the system is related to the number of pyrophosphates generated per pathogen (relative to the background detection limit of approximately 10^{-18} moles of ATP or pyrophosphate). By providing amplification primers that hybridize to captured DNA or RNA, theoretically 10^{-18} moles (one amol) or more of pyrophosphate can be produced from capture of a single organism. Thus a very small number of organisms can be detected by BRC amplified nucleic acid-based specific pathogen identification, similar to the sensitivity of BRC-enhanced ATP detection. Thus both ATP and nucleic acid-based detection allow detection of a small number of pathogens.

[00140] In BRC-amplified nucleic acid-based detection, amplification primers are designed to have sequences specific to the microbe of interest. The amplification primers are initially added into the solution in which the target pathogen is potentially present. In this case, the primers are added together with the reagents used in BRC-amplified detection of ATP. Hybridization occurs during the heating and subsequent cooling that occurs during the microbial lysis step. The hybridization phase allows for the annealing of the target to the surface via the capture probe and hybridization of the primer to the target DNA to form microbial nucleic acid/amplification primer complexes.

[00141] As the hybridized microbial nucleic acid/amplification primer complexes flow downstream from the microbial capture sites, free ends of the microbial DNA are able to hybridize to specific DNA probe capture sites that are placed downstream. Thereby if the target DNA is present in the test sample, the primer anneals to the specific capture site of the pathogen DNA. Further, the quantity of nucleic acid/amplification primer captured is related to the quantity of the primed pathogen DNA present in the sample and thereby related to the number of pathogen organisms present in the original sample. A polymerase enzyme is added together with the Mg-dNTP substrate for the polymerization reaction. The primers bound to the pathogen nucleic acid (DNA or RNA) are extended when nucleotides are incorporated during polymerization (FIG. 11). A single PPi molecule is generated for each nucleotide incorporated. If

the length of polymerized sequence is known, the quantity of the target pathogen can be quantified and its concentration determined.

[00142] The light intensity per unit volume generated in this process is given by:

$$I = \alpha \cdot \left(\frac{k_L}{V} \right) \cdot N_p \cdot L_x \quad (26)$$

where α is the quantum yield of the bioluminescence process, N_p the number of pathogens in the solution and L_x is the extendable length of the pathogen. The specificity of this method is determined by the specificity of the capture probe hybridization and the polymerization step of the primed DNA.

[00143] A variety of BRC amplification techniques may be utilized with nucleic acid based pathogen detection. For example, as shown in FIG. 4, a branched BRC assay may be performed to detect pathogen nucleic acids, increasing the number of PPi molecules released during the polymerization reaction. The amplification primers may be added subsequent to lysis and release of ATP by heat and sonication. A hybridization buffer carries the released nucleic acid to the downstream specific capture sites where they hybridize, if the appropriate nucleic acid sequence is present. The hybridization phase allows for the annealing of the target to the surface via the capture probe. The amplification primers help to increase the sensitivity since more pyrophosphate is liberated for each target DNA molecule hybridized. Alternatively, a transcription based method as illustrated in FIG. 5 may be used to amplify the signal detected from target pathogen nucleic acids. Tests may also be performed using PCR amplified DNA products from pathogens.

[00144] A possible limitation of this technique could be that the sequences of the pathogens need to be known *a priori*. Only pathogens to which the sequence is known can be detected. If an unknown pathogen is tested, although present in a sample, a negative result is obtained. One way to overcome this is to use conserved probe sequences to targets that are found in a broad category of pathogens, not an individual pathogen.

Microbial Class-Based Detection (Nucleotide Hybridization-Dependent)

[00145] In certain embodiments of the invention, BRC assays may be performed to quickly determine the class of pathogens present in a sample, such as gram-positive or gram-negative

bacterium, fungus, or virus. This class detection is useful for cases in which sample contains an unknown pathogen in one of those broad categories. In some cases, determination of the class of pathogen present may provide an early indication of the type of antibiotic that may be used to effectively treat an infection. Class identification may also be of use in biowarfare applications to assist in determining appropriate countermeasures.

[00146] Class-specific detection may be performed using nucleic acid sequences that are unique between the different classes, yet universal within each class. Such sequences may be used to design appropriate primers and/or capture probes. If a particular class of organism is present, the capture probes and/or primers bind and BRC or BRC amplification methods may be used to detect a pathogen nucleic acid. For example, tmRNA and rRNA sequences have been used to amplify a specific region of gram-positive bacterial nucleic acids (Schonhuber *et al.*, *BMC Microbiol* 1:20, 2001; Meier *et al.*, *Syst Appl Microbiol* 22:186-96, 1999). Primer sequences appropriate for amplification of fungal DNA have also been identified (Sandhu *et al.*, *J Clin Microbiol* 33:2913-9, 1995; Haynes *et al.*, *J Med Vet Mycol* 33:319-25, 1995). A universal viral DNA sequence has not yet been found, but sequences have been determined of use in identifying particular types of viruses, such as adenoviruses (Takeuchi *et al.*, *J Clin Microbiol* 37:1839-45, 1999) and human papilloma virus (Fernandez-Contreras *et al.*, *J Virol Methods* 87:171-5, 2000). Various sequences may be utilized for the identification of specific types of viruses in a sample.

[00147] Sample processing may occur as disclosed above. Once the organisms in a sample are lysed, nucleic acids are released and may be captured by class specific capture probes placed as an array downstream from the lysis sites. Release of cellular contents upon lysis may require additional sonication. Restriction endonucleases may be employed to enhance the capture of DNA (or RNA) by the immobilized capture probes. Endonucleases may also be utilized, for example, to converted circular nucleic acid molecules into linear molecules, providing 3' ends to allow terminal transferase activity to occur.

[00148] Once the sample nucleic acids are hybridized to immobilized capture probes, a mixture of specific amplification primers is added and allowed to bind to the immobilized nucleic acids. The primers can be extended by DNA polymerase to yield pyrophosphate, which is detected by BRC or BRC amplification methods as discussed above.

[00149] An advantage of the high gain of enhanced BRC in combination with nucleic acid amplification is that culture of microorganisms is not needed for their detection, identification and/or quantification. In this way rapid detection may be achieved with microorganisms concentrated directly from biological samples. The presence of an organism's DNA, such as a fungus or virus, can be detected specifically with the BRC assay in conjunction with the use of the specific capture probes and/or secondary primers. In alternative embodiments, it is possible to test for more than one sequence for each class of pathogen. This decreases the likelihood of a false-negative result.

Antibiotic Resistance Analysis with BRC

[00150] As presently performed, antibiotic resistance testing generally requires growth of the microbe on specialized media to obtain a sample large enough to test under different conditions. This initial growth period ranges from 24 hours to several days, depending upon the growth characteristics of the microbe. Once sufficient growth of the microbe has been obtained, the sample must be split among media plates containing different antibiotics. A visual observation of growth on the media plates is needed, again requiring additional time to allow for microbial growth in the presence of the various antibiotics. This delay results in problems ranging from unnecessary treatment of a patient to misdiagnoses and improper treatment detrimental to the patient. With the BRC assay, the delay in determining antibiotic susceptibility can be minimized.

[00151] The BRC assay can be used to detect very low levels of bacteria in a sample. This characteristic can be leveraged in an antibiotic resistance analysis to reduce the time required for such analyses. For example, after bacteria are determined to be present in a sample, additional aliquots from the original sample may be placed into separate wells containing different antibiotics (in the appropriate concentrations). The samples are allowed to grow, and the BRC-enhanced detection assay for pathogen nucleic acids can be performed after a short period of growth, such as a few hours. Due to the high sensitivity of the BRC assay, direct visual observation of growth is not necessary. Alternatively, as discussed above, the effect of antibiotics on bacterial ATP content may also be determined in a relatively short time period.

Thermostable Enzymes

[00152] In certain embodiments of the invention, the BRC assay and/or other detection methods may utilize thermostable enzymes, including but not limited to thermostable terminal

transferase, DNA polymerase, RNA polymerase, reverse transcriptase, ATP sulfurylase and/or luciferase. Such thermostable enzymes may be of use for a variety of applications. Use of thermostable polymerases for thermal cycling processes, such as PCR, are well known in the art. In some embodiments, where detection of light emission or another type of signal occurs in real time, such thermal cycling processes may occur concurrently with BRC detection or other detection modalities. In such cases, thermostable detection enzymes such as luciferase and ATP sulfurylase may be utilized to avoid thermal inactivation during the PCR process. Alternatively, isothermal processes for nucleic acid and/or oligonucleotide amplification and/or detection may be conducted at elevated temperatures, utilizing thermostable enzymes. In certain embodiments, the use of thermostable enzymes would allow nucleic acid and/or oligonucleotide polymerization and detection to occur in a single step process, avoiding the need to separate the production of PPi or ATP from their detection.

[00153] Any thermostable enzyme known in the art may be utilized. Such enzymes are commercially available from a variety of sources, such as *Taq* polymerase (Roche Molecular Biochemicals, Indianapolis, IN), KlenTaq™ DNA Polymerase (Sigma-Aldrich, St. Louis, MO), *Tgo* DNA Polymerase (Roche Molecular Biochemicals), DyNAzyme™ DNA Polymerase (Finnzymes, Espoo, Finland) and GeneAmp® thermostable reverse transcriptase (Applied Biosystems, Foster City, CA). A thermostable form of luciferase (Ultraglow™ recombinant luciferase, Promega Corp., Madison, WI, catalog #E140X) has been found by the inventors to be stable to about 95°C. *Taq* polymerase is a thermostable enzyme with terminal transferase activity.

[00154] A thermostable form of ATP sulfurylase has recently been reported (Hanna *et al.*, *Arch. Biochem. Biophys.* 406:275-288, 2002). The open reading frame encoding the thermostable enzyme is available from GenBank (Accession No. AAC07134). Methods of preparation and purification of thermostable ATP sulfurylase are known (Hanna *et al.*, 2002).

Apparatus for BRC Assays

[00155] To determine the quantity of PPi and/or ATP molecules present in BRC assays, the number of photons generated by the BRC process may be counted in selected time intervals, and the acquired waveform may be correlated to the target characteristics and/or quantity. The generation of photons by luciferase in typical BRC assays has a quantum efficiency (Q.E.) of

approximately 0.88 per consumed ATP molecule, and a maximum wavelength (depending on the type of luciferase) in the visible range of the electromagnetic spectrum (e.g. 565 nm for firefly luciferase).

[00156] Establishing a controlled environment for the BRC assay facilitates reliable measurement of the photon generation rate and subsequent target cell or pathogen quantification. In certain preferred embodiments of the invention, the use of a reaction chamber with controllable temperature and minimum background light may be important for accurate target cell or pathogen quantification. In an exemplary embodiment illustrated in FIG. 12, an apparatus for BRC detection may comprise one or more of the following components.

- i. Reaction chambers for BRC assay process, and/or affinity capture of targets
- ii. Fluidic system to insert reagents or extract products from the reaction chambers
- iii. Magnetic capturing devices
- iv. Vibration generator and/or mixing device
- v. Optical coupling devices to convey the generated photons to a photodetector
- vi. Photodetector to generate a relative photocurrent from the incident photons produced by BRC.
- vii. Sensor array to efficiently acquire and measure photocurrent
- viii. Cooling and/or heating device for controlling the reaction chamber temperature
- ix. Cooling and/or heating device for controlling the photodetector and/or sensor temperature
- x. Temperature controller module with a plurality of localized temperature sensors within the system to adjust the temperature based on user specifications.
- xi. Data acquisition hardware to digitize the data from the sensor array

Reaction Chambers

[00157] In certain embodiments of the invention, a reaction chamber may contain reaction buffer, substrates, enzymes and reagents for the BRC or other detection assays. Alternatively, the reaction chamber may contain capture medium to allow target cells or pathogens to be specifically captured using different types of affinity matrices, functionalized gels and/or probes immobilized on solid surfaces (e.g. magnetic beads). Various methods of specific cell or pathogen capture, such as antibody binding, aptamer binding, *etc.* are known in the art and any

such known method may be used. Exemplary methods for preparing one or more binding moieties, such as antibodies or aptamers, for capture of target cells or pathogens are discussed in more detail below.

[00158] The volume of the reaction chamber can vary anywhere between 1 nl (nanoliter) and 10 ml, but in most applications is typically between 2 μ l (microliters) and 50 μ l. In various embodiments, the reaction chamber may have an internal volume of about 1, 2, 5, 10, 20, 50, 100, 250, 500 or 750 nl, about 1, 2, 5, 10, 20, 50, 100, 250, 500 or 750 μ l, or about 1, 2, 5 or 10 ml. The reaction chamber can comprise 96 well, 384 well, or other standard microtiter plates, and may be microfabricated by standard methods (e.g. etched, molded, drilled) in glass, silicon, ceramic, plastic, or composite materials. In preferred embodiments, the material used to construct the reaction chamber is optically transparent to allow detection of bioluminescence. The distance between chambers can vary from about 10 μ m to about 5 cm, but in typical applications the distance will range between about 100 μ m and about 1 cm. Each chamber may have a plurality of inlets and outlets, and may also be connected to other chambers by channels. In certain embodiments, different reactions and/or assay procedures may be performed sequentially in different chambers. For example, a first chamber may contain a target capturing matrix (e.g., aptamer, lectin, antibody) specific for a given target cell or pathogen. After capture of the specific target cell or pathogen, other target cells or pathogens that do not bind may be washed out and sent to a second chamber, which might contain other types of specific capturing matrices, resulting in a chamber-specific (site-specific) capture of different targets within a mono-directional or bi-directional flow-through system.

Fluidic Systems

[00159] A fluidic system may comprise components that facilitate the movement of solutions (e.g. reaction buffer) and/or gases (e.g. oxygen for luciferin oxidation) into and/or out of reaction chambers through specific inlets and/or outlets. The fluidic system typically comprises a plurality of pumps, fluidic channels, valves, and/or fluid reservoirs. The fluidic system is capable of delivering and/or extracting solutions or gases of volumes of about 1 pl to about 10 ml, but in typical applications the volume transferred at any given time will vary between about 1 nl to about 20 μ l. The fluidic system may also be used to deliver and/or remove biological samples, magnetic particles, BRC or other reagents, primers, antibodies, *etc.* into the chambers.

Magnetic Capture Device

[00160] In particular embodiments of the invention, magnetic particles such as paramagnetic beads coated with capture (binding) moieties may be used to capture specific targets. In such embodiments, a magnetic field is generally induced to capture beads attached to target cells or pathogens and to wash out uncaptured species using a fluidic system. The magnetic field and/or fluidic system may also be used to move the beads to particular spatial locations at different points during the procedure. The magnetic field within the chambers and/or fluidic channels can be created by a plurality of independent permanent magnets, magnetic coils, and/or magnetic spiral inductors. In some embodiments of the invention the magnetic field intensity introduced on the field generator within the chamber may be modulated in order to release and capture the magnetic particles. In these cases, a permanent magnet can be mechanically placed in close proximity and/or into the designated chamber to capture beads, or moved away from the chamber to release beads. In the case of magnetic coils or spiral inductors, the release and capture of magnetic beads can be carried out by controlling the electrical current driving the coil or spiral.

[00161] Magnetic particles, including magnetic particles derivatized for attachment of specific capture (binding) moieties, may be purchased, for example from Dynal Biotech (Dynabeads®, Lake Success, NY). Alternatively, magnetic beads may be prepared by known methods (*e.g.*, U.S. Pat. No. 4,267,234). Processes for the coupling of molecules to magnetic beads or a magnetite substrate are well known in the art (*i.e.* U.S. Patent Nos. 4,695,393, 3,970,518, 4,230,685, and 4,677,055).

Vibration Generator and/or Mixing Device

[00162] In certain embodiments of the invention, mechanical motion may be used to stir, pump, filter, and/or manipulate gases, liquids, cells, bacteria, and other samples. In some applications electromechanical actuators and/or ultrasonic devices may be used to induce motion and/or create mechanical waves in the chamber and/or channels of the apparatus. Such devices may also affect the BRC or other reaction process. Electromechanical actuators are known in the art and may be purchased from standard sources.

Optical Coupling Device

[00163] Light that is generated from the reaction chambers, for example by BRC assay, may be collected and transferred to a photodetector using an optical coupling device. In alternative embodiments of the invention, the generated photons may either propagate for a short distance to a photodetector or may reach a photodetector substantially in contact with the chamber wall (distance from detector to chamber can vary from $1\mu\text{m}$ to 1 m, but typically would range from $10\mu\text{m}$ to 2 mm), or can be guided using an optical waveguide system (e.g. single optical fiber, or fiber bundle). In addition, different variations of lenses and/or mirrors may also be used to focus the generated light onto a photodetector device. An optical coupling device may also comprise one or more filters, which only pass certain wavelength regions relevant to the assay detection (e.g. 550 nm to 570 nm for Firefly luciferase photon emission). Optical fibers and other types of optical coupling devices are well known in the art and any such known device may be used in the disclosed apparatus.

Photodetector and Sensor Array

[00164] A number of different photosensitive devices can be used to measure the photon flux intensity from BRC or other optical assay. The devices can be photodiodes, avalanche photodiodes, phototransistors, vacuum photodiodes, silicon photodiodes, photomultiplier tubes (PMTs), multianode photomultiplier tubes, charged-coupled devices (CCDs), CCD cameras, CMOS image sensors, photoresistive materials or any other optical detection device known in the art. The photodetector can be in a 2D array format, where an individual or plurality of sensors within the array measures the emitted light from a chamber selected from a plurality of reaction chambers. In certain embodiments a single photodetector can be used to sequentially measure light from multiple chambers, one (or several) at a time, in a sequential fashion. In some embodiments, the photodetector can be in close proximity to the chamber and/or even integrated onto the chambers. As an example one could use an array of photodiodes in silicon wafers, where chambers are etched into either the oxide top layers, or the bulk silicon wafer. As another example a micro-fluidic chip can be used, where the reaction chambers are connected via micro-channels and the whole chip is put onto the surface of a semiconductor based image sensor (e.g. CMOS or CCD), where the light from each well directly impinges on a photosensitive section of the imager.

[00165] In certain embodiments of the invention, a highly sensitive cooled CCD detector may be used. The cooled CCD detector has a probability of single-photon detection of up to 80%, a high spatial resolution pixel size (5 microns), and sensitivity in the visible through near infrared spectra. (Sheppard, *Confocal Microscopy: Basic Principles and System Performance in: Multidimensional Microscopy*, P.C. Cheng *et al.* eds., Springer-Verlag, New York, NY pp. 1-51, 1994.) In another embodiment of the invention, a coiled image-intensified coupling device (ICCD) may be used as a photodetector that approaches single-photon counting levels (U.S. Pat. No. 6,147,198). A small number of photons triggers an avalanche of electrons that impinge on a phosphor screen, producing an illuminated image. This phosphor image is sensed by a CCD chip region attached to an amplifier through a fiber optic coupler.

[00166] In some embodiments of the invention, an avalanche photodiode (APD) may be made to detect low light levels. The APD process uses photodiode arrays for electron multiplication effects (U.S. Pat. No. 6,197,503). The invention is not limited to the disclosed embodiments and it is contemplated that any light detector known in the art that is capable of accumulating photons over a time interval may be used in the disclosed methods and apparatus.

[00167] The output of the photodetector is typically in form of a photocurrent and/or voltage, which has a relationship to the incident photon flux to the detector. The output of the sensor depends on the topology, number of photodetector elements and characteristics of individual photodetectors, and may be in parallel (*i.e.* all output channels are on separate lines), or sequential (*i.e.* one output is connected to the output line at a time).

Temperature Control Devices

[00168] In some embodiments of the invention, the reaction chambers and/or photosensors are designed to be temperature controlled, for example by incorporation of Peltier elements or other methods known in the art. Methods of controlling temperature for low volume liquids used in nucleic acid polymerization or other reactions are known in the art. (See, *e.g.*, U.S. Patent Nos. 5,038,853, 5,919,622, 6,054,263 and 6,180,372.) Methods for maintaining temperature control of sensing elements are also known in the art.

[00169] In certain embodiments of the invention, cyclic changes in temperature in one or more reaction chambers (*e.g.*, as used in the PCR process) may be useful. The temperature profile can vary from 0°C and 100°C, but in most BRC applications varies between room

temperature and 95°C. Each chamber may be individually thermally controlled, for example with a different heater/cooler device and a temperature sensor (e.g. thermocouple, or a thermistor) associated with each chamber. Alternatively, a plurality of chambers may be commonly thermally controlled, using a single temperature controller and sensor.

[00170] Different types of known heating and/or cooling devices may be used, such as resistive heaters, Peltier devices, heat sinks, fluidic cooling and heating devices and laser cooling and heating. As an example, Peltier devices, also known as thermoelectric (TE) modules, are small solid-state devices that function as heat pumps, transferring heat from one location to another. Peltier devices may be incorporated into an apparatus in contact with the reaction chambers to form a temperature-controlled reaction chamber unit. A typical Peltier unit is a few millimeters thick by a few millimeters to a few centimeters square. It is a sandwich formed by two ceramic plates with an array of small bismuth telluride cubes ("couples") in between. When a direct current (DC) is applied, heat is pumped from one side of the unit to the other, at which point the heat can be removed with a heat sink or other cooling means. Heat may be pumped in either direction, allowing alternate heating or cooling of the chamber.

[00171] A heating or cooling module may also be used to control the temperature of the photosensors (e.g. photodiodes) used in the system. The performance of photodiodes, for example, is extremely dependent upon temperature. Temperature can affect both the quantum efficiency and even more dramatically the dark current and therefore the noise characteristics of such photosensors. In preferred embodiments of the invention, the sensors will have a fixed temperature during measurements of light emission. A cooling/heating device may be either integrated with, or put into contact with, the photosensor in order to maintain a predetermined temperature or a time-dependent temperature cycle.

Thermal Controller

[00172] The heating and cooling devices may be individually controlled by a controller means. In the case of TE cooling, an electronic controller module may sense the temperature of each designated heating/cooling location. Based on the difference between the actual and predetermined temperature, the controller pumps heat into or out of the location until the location temperature reaches its predetermined (null point) value. The controller means in turn may be controlled by a computer or similar secondary controller device, having a user interface so that a

predetermined temperature, or predetermined series of temperatures, or predetermined cycles of a repeated temperature series may be selected by the user. Such computer systems and temperature controller means are well known in the art and can incorporate any of a wide variety of temperature-control devices well known to those skilled in the art.

[00173] Certain embodiments of the invention concern a portable, ultra-sensitive, pathogen detection system that can identify predetermined pathogens and their antibiotic resistance profiles in biological samples. Applications of this device include detection and quantification of the presence of predetermined microbe species in air or sterile biological fluids such as blood, cerebrospinal fluid and urine. Detection can be performed in a much more rapid and accurate fashion than is currently possible. Such systems may comprise an apparatus as disclosed herein, designed for use as a microfluidic system.

Microfluidic Structures

[00174] In various embodiments of the invention, microfluidic devices may be used to provide samples to specific capture sites and to process such samples for target cell or pathogen detection. The small volumes of microfluidic devices allow processing of small sample volumes. Given the small detection volumes for BRC assays, background luminescence from the system will also be low. The combination of a low sample volume and low background luminescence allows for particularly high sensitivity of detection. Microfluidic devices comprise one or more channels of micron-size depth and width, generally between 10 and 900 microns. The channels may be of varying length but generally are between 0.1 and 100 cm in length. Microfluidic devices therefore contain very small volumes defined by each channel, generally ranging from 100 picoliters to 100 microliters. Because of their small internal volumes, reagent consumption is low, only a few target cells or pathogens are required to create a measurable signal, the devices are compact and easily stored and transported, and the devices may be designed to be disposable and convenient to use.

[00175] Low reagent consumption is especially important when expensive or difficult to obtain reagents are used. When used, for example, for pathogen detection, the number of microorganisms required to be detected can be very low, allowing detection limits for example of a single cell, 2 or more cells, 10 cells, 100 cells or 1000 cells. The microfluidic channels may be formed from any substance having a surface compatible with biological materials. In

exemplary embodiments of the invention, the channels (or at least the surface of the channels) may be made of glass, fused silica, quartz or silicon. (See, *e.g.*, Bousse *et al.*, "Electrokinetically Controlled Microfluidic Analysis Systems," *Ann. Rev. Biophys. Biomol. Struct.* 29:155-181, 2000.)

[00176] Other materials that may be used for construction of microfluidic devices include organic polymers (*i.e.* plastics) such as methacrylates, polystyrene, polypropylene, polycarbonate, polyethylene, or the like. Soft polymeric materials such as organosilanes, including polydimethylsilane (PDMS) can be used to fabricate the microfluidic channels. The soft polymers alternatively may be polyacrylamide materials or mixed polymers containing copolymerized organic or inorganic substances. An advantage of soft polymers is that they are deformable by applying external pressure. Application of external pressure results in creation of a closed valve. Because the soft polymer materials can be elastic, release of the pressure results in reopening of the valve. Flow in the channel is restored provided that a gradient in pressure is created along the length of the channel. (See, *e.g.*, Thorsen *et al.*, "Microfluidic Large-Scale Integration," *Science* 298:580-586, 2002.) Application of external pressure adjacent to a closed valve creates pressure that may be used to pump fluids. Alternatively, the pressure may be created by application of gas pressure, application of a vacuum (relative to ambient pressure) or by applying an electrical field along the channel and creating a pressure gradient by electroendosmosis. All of these processes are well known in the art.

Micro-Electro-Mechanical Systems (MEMS)

[00177] In some embodiments of the invention, the chambers, sensors and other components of the disclosed apparatus may be incorporated into one or more Micro-Electro-Mechanical Systems (MEMS). MEMS are integrated systems that may comprise mechanical elements, actuator elements, control elements, detector elements and/or electronic elements. All of the components may be manufactured by known microfabrication techniques on a common chip, comprising a silicon-based or equivalent substrate (*e.g.*, Voldman *et al.*, *Ann. Rev. Biomed. Eng.* 1:401-425, 1999).

[00178] The electronic components of MEMS may be fabricated using integrated circuit (IC) processes (*e.g.*, CMOS, Bipolar, or BICMOS processes). They may be patterned using photolithographic and etching methods known for semiconductor chip manufacture. The

micromechanical components may be fabricated using "micromachining" processes that selectively etch away parts of the silicon wafer and/or add new structural layers to form the mechanical and/or electromechanical components. Basic techniques in MEMS manufacture include depositing thin films of material on a substrate, applying a patterned mask on top of the films by photolithographic imaging or other known lithographic methods, and selectively etching the films. A thin film may have a thickness in the range of a few nanometers to 100 micrometers. Deposition techniques of use may include chemical procedures such as chemical vapor deposition (CVD), electrodeposition, epitaxy and thermal oxidation and physical procedures like physical vapor deposition (PVD) and casting. Sensor layers of 5 nm thickness or less may be formed by such known techniques. Standard lithography techniques may be used to create sensor layers of micron or sub-micron dimensions, operably coupled to detectors.

[00179] The manufacturing method is not limiting and any methods known in the art may be used, such as atomic layer deposition, pulsed DC magnetron sputtering, vacuum evaporation, laser ablation, injection molding, molecular beam epitaxy, dip-pen nanolithography, reactive-ion beam etching, chemically assisted ion beam etching, microwave assisted plasma etching, focused ion beam milling, electron beam or focused ion beam technology or imprinting techniques. Methods for manufacture of nanoelectromechanical systems may be used for certain embodiments of the invention. (See, *e.g.*, Craighead, Science 290:1532-36,0.)

[00180] In some embodiments, the reaction chamber and other components of the apparatus may be manufactured as a single integrated chip. Such a chip may be manufactured by methods known in the art, such as by photolithography and etching. However, the manufacturing method is not limiting and other methods known in the art may be used, such as laser ablation, injection molding, casting, or imprinting techniques. Microfabricated chips are commercially available from sources such as Caliper Technologies Inc. (Mountain View, CA) and ACLARA BioSciences Inc. (Mountain View, CA).

[00181] In a non-limiting example, Borofloat glass wafers (Precision Glass & Optics, Santa Ana, CA) may be pre-etched for a short period in concentrated HF (hydrofluoric acid) and cleaned before deposition of an amorphous silicon sacrificial layer in a plasma-enhanced chemical vapor deposition (PECVD) system (PEII-A, Technics West, San Jose, CA). Wafers may be primed with hexamethyldisilazane (HMDS), spin-coated with photoresist (Shipley 1818,

Marlborough, MA) and soft-baked. A contact mask aligner (Quintel Corp. San Jose, CA) may be used to expose the photoresist layer with one or more mask designs, and the exposed photoresist removed using a mixture of Microposit developer concentrate (Shipley) and water. Developed wafers may be hard-baked and the exposed amorphous silicon removed using CF₄ (carbon tetrafluoride) plasma in a PECVD reactor. Wafers may be chemically etched with concentrated HF to produce the reaction chamber and any channels. The remaining photoresist may be stripped and the amorphous silicon removed.

[00182] Access holes may be drilled into the etched wafers with a diamond drill bit (Crystalite, Westerville, OH). A finished chip may be prepared by thermally bonding an etched and drilled plate to a flat wafer of the same size in a programmable vacuum furnace (Centurion VPM, J. M. Ney, Yucaipa, CA). In certain embodiments, the chip may be prepared by bonding two etched plates to each other. Alternative exemplary methods for fabrication of a reaction chamber chip are disclosed in U.S. Patent Nos. 5,867,266 and 6,214,246.

Nucleic Acids and Oligonucleotides

[00183] In various embodiments of the invention, pathogen nucleic acids may be prepared by any technique known in the art. In certain embodiments, analysis may be performed on crude sample extracts, containing complex mixtures of nucleic acids, proteins, lipids, polysaccharides and other compounds. Such samples are likely to contain contaminants that could potentially interfere with the BRC process or other detection methods. In preferred embodiments, pathogen nucleic acids may be partially or fully separated from other sample constituents before analysis.

[00184] Methods for partially or fully purifying DNA and/or RNA from complex mixtures, such as cell homogenates or extracts, are well known in the art. (See, *e.g.*, Guide to Molecular Cloning Techniques, eds. Berger and Kimmel, Academic Press, New York, NY, 1987; Molecular Cloning: A Laboratory Manual, 2nd Ed., eds. Sambrook, Fritsch and Maniatis, Cold Spring Harbor Press, Cold Spring Harbor, NY, 1989). Generally, cells, tissues or other source material containing nucleic acids are first homogenized, for example by freezing in liquid nitrogen followed by grinding in a mortar and pestle. Certain tissues may be homogenized using a Waring blender, Virtis homogenizer, Dounce homogenizer or other homogenizer. Crude homogenates may be extracted with detergents, such as sodium dodecyl sulphate (SDS), Triton X-100, CHAPS (3-[(3-cholamidopropyl)-dimethylammonio]-1-propane sulfonate),

octylglucoside or other detergents known in the art. As is well known, nuclease inhibitors such as RNase or DNase inhibitors may be added to prevent degradation of pathogen nucleic acids.

[00185] Extraction may also be performed with chaotropic agents such as guanidinium isothiocyanate, or organic solvents such as phenol. In some embodiments, protease treatment, for example with proteinase K, may be used to degrade cell proteins. Particulate contaminants may be removed by centrifugation or ultracentrifugation. Dialysis against aqueous buffer of low ionic strength may be of use to remove salts or other soluble contaminants. Nucleic acids may be precipitated by addition of ethanol at -20°C, or by addition of sodium acetate (pH 6.5, about 0.3 M) and 0.8 volumes of 2-propanol. Precipitated nucleic acids may be collected by centrifugation or, for chromosomal DNA, by spooling the precipitated DNA on a glass pipet or other probe. The skilled artisan will realize that the procedures listed above are exemplary only and that many variations may be used, depending on the particular type of nucleic acid to be analyzed.

[00186] In certain embodiments, nucleic acids to be analyzed may be naturally occurring DNA or RNA molecules. Virtually any naturally occurring nucleic acid may be analyzed by the disclosed methods including, without limit, chromosomal, mitochondrial or chloroplast DNA or ribosomal, transfer, heterogeneous nuclear or messenger RNA. Nucleic acids may be obtained from either prokaryotic or eukaryotic sources by standard methods known in the art. Alternatively, nucleic acids of interest may be prepared artificially, for example by PCR™ or other known amplification processes or by preparation of libraries such as BAC, YAC, cosmid, plasmid or phage libraries containing nucleic acid inserts. (See, *e.g.*, Berger and Kimmel, 1987; Sambrook *et al.*, 1989.) The source of the nucleic acid is unimportant for purposes of analysis and it is contemplated within the scope of the invention that nucleic acids from virtually any source may be analyzed.

Nucleic Acid Replication

[00187] In certain embodiments of the invention, pathogen nucleic acids may be amplified and/or replicated prior to or during detection. Amplification may be accomplished by any technique known in the art. Exemplary embodiments are disclosed below.

Primers

[00188] The term primer, as used herein, is meant to encompass any nucleic acid that is capable of priming the synthesis of a nascent nucleic acid in a template-dependent process. Typically, primers are oligonucleotides from ten to twenty base pairs in length, but longer sequences may be employed. Primers may be provided in double-stranded or single-stranded form, although the single-stranded form is preferred. Primers may be prepared, for example, using oligonucleotide synthesizers available from standard commercial sources (*e.g.*, Applied Biosystems, Foster City, CA). Alternatively, primers of any selected sequence may be obtained from standard commercial sources (*e.g.*, Midland Certified Reagents, Midland, TX). Such commercial primers may be purchased with specific chemical modifications, for example, attachment of a biotin moiety or other reactive group to facilitate immobilization of the primer to a solid surface or attachment of a label or other group. In certain embodiments of the invention, primers incorporating a preexisting label moiety may be purchased from commercial sources. Methods for selection, design and validation of primer sequences to amplify any given pathogen nucleic acid and/or oligonucleotide tag sequence are well known in the art.

Polymerases

[00189] In certain embodiments of the invention, the disclosed methods may involve binding of a DNA polymerase to a primer molecule and the catalyzed addition of nucleotide precursors to the 3' end of a primer. In alternative embodiments, other types of polymerase, such as RNA polymerase, may be utilized that do not require primers but rather bind to promoter sequences to initiate RNA polymerization. Non-limiting examples of polymerases of potential use include DNA polymerases, RNA polymerases, reverse transcriptases, and RNA-dependent RNA polymerases. The differences between these polymerases in terms of their requirement or lack of requirement for primers or promoter sequences are known in the art.

[00190] Non-limiting examples of polymerases that may be of use include *Thermatoga maritima* DNA polymerase, AmplitaqFS™ DNA polymerase, Taqenase™ DNA polymerase, ThermoSequenase™, Taq DNA polymerase, Qbeta™ replicase, T4 DNA polymerase, *Thermus thermophilus* DNA polymerase, RNA-dependent RNA polymerase and SP6 RNA polymerase. Commercially available polymerases including Pwo DNA Polymerase from Boehringer Mannheim Biochemicals (Indianapolis, IN); Bst Polymerase from Bio-Rad Laboratories

(Hercules, CA); IsoTherm™ DNA Polymerase from Epicentre Technologies (Madison, WI); Moloney Murine Leukemia Virus Reverse Transcriptase, *Pfu* DNA Polymerase, Avian Myeloblastosis Virus Reverse Transcriptase, *Thermus flavus* (*Tfl*) DNA Polymerase and *Thermococcus litoralis* (*Tli*) DNA Polymerase from Promega (Madison, WI); RAV2 Reverse Transcriptase, HIV-1 Reverse Transcriptase, T7 RNA Polymerase, T3 RNA Polymerase, SP6 RNA Polymerase, RNA Polymerase E. coli, *Thermus aquaticus* DNA Polymerase, T7 DNA Polymerase +/- 3'→5' exonuclease, Klenow Fragment of DNA Polymerase I, Thermus 'ubiquitous' DNA Polymerase, and DNA polymerase I from Amersham Pharmacia Biotech (Piscataway, NJ).

[00191] As is known in the art, various polymerases have an endogenous 3'-5' exonuclease activity that may be used for proof-reading newly incorporated nucleotides. Because a molecule of pyrophosphate is generated for each nucleotide incorporated into a growing chain, regardless of whether or not it is subsequently removed, in certain embodiments of the invention it may be preferred to use polymerases that are lacking exonuclease or proof-reading activity. Methods of using polymerases and compositions suitable for use in such methods are well known in the art (*e.g.*, Berger and Kimmel, 1987; Sambrook *et al.*, 1989).

Amplification Methods

[00192] A number of template dependent processes are available to amplify pathogen nucleic acids. One of the best known amplification methods is the polymerase chain reaction (referred to as PCR™) which is described in U.S. Patent Nos. 4,683,195, 4,683,202 and 4,800,159, and in Innis *et al.* (*PCR Protocols*, Academic Press, Inc., San Diego CA, 1990).

[00193] Briefly, in PCR, two primer sequences are prepared which are complementary to regions on opposite complementary strands of, for example, a pathogen nucleic acid. An excess of deoxynucleoside triphosphates are added to a reaction mixture along with a DNA polymerase, *e.g.*, *Taq* polymerase. If the target sequence is present in a sample, the primers will bind to the target and the polymerase will cause the primers to be extended along the target sequence by adding on nucleotides. By raising and lowering the temperature of the reaction mixture, the extended primers will dissociate from the nucleic acid to form reaction products, excess primers will bind to the nucleic acid and to the reaction products and the process is repeated.

[00194] A reverse transcriptase PCR amplification procedure may be performed in order to amplify mRNA. Methods of reverse transcribing RNA into cDNA are well known and disclosed, for example, in Sambrook *et al.* (1989). Alternative methods for reverse transcription utilize thermostable DNA polymerases. These methods are disclosed in WO 90/07641 filed December 21, 1990. Polymerase chain reaction methodologies are well known in the art.

[00195] Qbeta Replicase, disclosed in PCT Application No. PCT/US87/00880, may also be used for amplification. In this method, a replicative sequence of RNA which has a region complementary to that of a pathogen nucleic acid is added to a sample in the presence of an RNA polymerase. The polymerase will copy the replicative sequence which may then be detected.

[00196] Strand Displacement Amplification (SDA) is an isothermal method of carrying out amplification of pathogen nucleic acids that involves multiple rounds of strand displacement and synthesis, *i.e.*, nick translation. A similar method, called Repair Chain Reaction (RCR), involves annealing several probes throughout a region targeted for amplification, followed by a repair reaction.

[00197] Still other amplification methods are disclosed in GB Application No. 2 202 328, in which "modified" primers are used in a PCR like process. The primers may be modified by labeling with a capture moiety (*e.g.*, biotin) and/or a detector moiety (*e.g.*, enzyme). Other nucleic acid amplification procedures include transcription-based amplification systems (TAS), nucleic acid sequence based amplification (NASBA) and 3SR. (See, Kwoh *et al.*, *Proc. Nat. Acad. Sci. USA*, 86: 1173, 1989) and PCT Application WO 88/10315.) These amplification techniques involve annealing a primer which has pathogen nucleic acid specific sequences. Following polymerization, DNA/RNA hybrids are digested with RNase H while double stranded DNA molecules are heat denatured again. In either case the single stranded DNA is made fully double stranded by addition of second pathogen nucleic acid specific primer, followed by polymerization. The double-stranded DNA molecules are then multiply transcribed by a polymerase such as T7 or SP6. In an isothermal cyclic reaction, the RNA's are reverse transcribed into double stranded DNA, and transcribed once again with a polymerase such as T7 or SP6.

[00198] Davey *et al.*, European Application No. 329 822 disclose a nucleic acid amplification process involving cyclically synthesizing single-stranded RNA ("ssRNA"), ssDNA, and double-stranded DNA (dsDNA). The ssRNA is a first template for a first primer oligonucleotide, which

is elongated by reverse transcriptase. The RNA is then removed from the resulting DNA:RNA duplex by the action of ribonuclease H. The resultant ssDNA is a second template for a second primer, which also includes the sequences of an RNA polymerase promoter (exemplified by T7 RNA polymerase) 5' to its homology to the template. This primer is then extended by DNA polymerase, resulting in a double-stranded DNA ("dsDNA") molecule having a sequence identical to that of the original RNA between the primers and having additionally, at one end, a promoter sequence. This promoter sequence may be used by the appropriate RNA polymerase to make many RNA copies of the DNA. These copies may then re-enter the cycle, leading to very swift amplification. With proper choice of enzymes, this amplification may be done isothermally without addition of enzymes at each cycle. Because of the cyclical nature of this process, the starting sequence may be chosen to be in the form of either DNA or RNA.

[00199] Miller *et al.*, PCT Application WO 89/06700 disclose a nucleic acid sequence amplification scheme based on the hybridization of a promoter/primer sequence to a single-stranded DNA ("ssDNA") followed by transcription of many RNA copies of the sequence. This scheme is not cyclic, *i.e.*, new templates are not produced from the resultant RNA transcripts. Other amplification methods including "race" and "one-sided PCR" are known in the art and any such known method may be used. (See, *e.g.*, Frohman, *In: PCR™ Protocols: A Guide To Methods And Applications*, Academic Press, N.Y., 1990; Ohara *et al.*, *Proc. Nat'l Acad. Sci. USA*, 86:5673-5677, 1989).

[00200] Kurn *et al.* (U.S. Patent No. 6,251,639) disclose an isothermal, single primer linear nucleic acid amplification method. In this approach, methods for amplifying complementary DNA using a composite primer, primer extension, strand displacement, and optionally a termination sequence, are provided, as well as methods for amplifying sense RNA using a composite primer, primer extension, strand displacement, optionally template switching, a propromoter oligonucleotide and transcription.

Promoters

[00201] In various embodiments of the invention involving transcription of a DNA strand by an RNA polymerase, it may be desirable to incorporate a promoter sequence, for example into a primer. A "promoter" refers to a DNA sequence recognized by an RNA polymerase to initiate transcription. Depending on the application, a promoter may be a eukaryotic promoter or a

prokaryotic promoter, to be used respectively with eukaryotic or prokaryotic RNA polymerases. Promoter elements recognized by eukaryotic and prokaryotic RNA polymerases are known in the art and any such known elements may be used.

[00202] The term promoter refers generically to a group of transcriptional control modules that are clustered around the initiation site for RNA polymerase. Promoters are composed of discrete functional modules, each consisting of approximately 7-20 bp of DNA, and containing one or more recognition sites for transcriptional activator or repressor proteins. At least one module in each promoter functions to position the start site for RNA synthesis. The best known example of this is the TATA box (or Pribnow box in prokaryotes), but in some promoters lacking a TATA box, a discrete element overlying the start site helps to fix the place of initiation.

[00203] Additional promoter elements regulate the frequency of transcriptional initiation. Typically, these are located in the region 30-110 bp upstream of the start site, although a number of promoters have been shown to contain functional elements downstream of the start site as well. The spacing between promoter elements frequently is flexible, so that promoter function is preserved when elements are inverted or moved relative to one another.

[00204] The particular promoter that is employed to initiate transcription is not believed to be important. In various embodiments, the human cytomegalovirus (CMV) immediate early gene promoter, the SV40 early promoter or the Rous sarcoma virus long terminal repeat can be used to obtain high-level transcription by eukaryotic RNA Polymerase II. The use of other viral, mammalian or bacterial promoters which are well-known in the art is also contemplated. Any promoter/enhancer combination (*e.g.*, Eukaryotic Promoter Data Base) could be used to drive transcription of a pathogen nucleic acid sequence.

[00205] Tables 3 and 4 list various eukaryotic enhancers/promoters that may be employed to regulate transcription. Enhancers are genetic elements that increase transcription from a eukaryotic promoter located at a distant position on the same molecule of DNA. Enhancers are organized much like promoters. That is, they are composed of many individual elements, each of which binds to one or more transcriptional proteins. The skilled artisan will recognize that in addition to the listed promoters/enhancers, many prokaryotic promoters are known and may be used to drive transcription. Such prokaryotic promoter sequences include, but are not limited to, the *lac* promoter, the *B-gal* promoter, the lambda promoter, the fd promoter, the *trp* promoter,

the T7 promoter, *etc.* Many prokaryotic promoters are commercially available from standard sources. Inducible promoter elements are disclosed in Table 4. In some embodiments of the invention, it may be preferable to activate transcription at specific points in the procedure. In such case, use of an inducible promoter allows precise control of the timing of RNA polymerase activity.

TABLE 3

ENHANCER/PROMOTER
Immunoglobulin Heavy Chain
Immunoglobulin Light Chain
T-Cell Receptor
HLA DQ α and DQ β
β -Interferon
Interleukin-2
Interleukin-2 Receptor
MHC Class II 5
MHC Class II HLA-DR α
β -Actin
Prealbumin (Transthyretin)
Muscle Creatine Kinase
Elastase I
Metallothionein
Collagenase
Albumin Gene
α -Fetoprotein
τ -Globin
β -Globin
e-fos
c-HA-ras
Insulin
Neural Cell Adhesion Molecule (NCAM)
α 1-Antitrypsin
H2B (TH2B) Histone
Mouse or Type I Collagen
Glucose-Regulated Proteins (GRP94 and GRP78)

ENHANCER/PROMOTER

Rat Growth Hormone
Human Serum Amyloid A (SAA)
Troponin I (TN I)
Platelet-Derived Growth Factor
Duchenne Muscular Dystrophy
SV40
Polyoma
Retroviruses
Papilloma Virus
Hepatitis B Virus
Human Immunodeficiency Virus
Cytomegalovirus

TABLE 4

Element	Inducer
MT II	Phorbol Ester (TPA) Heavy metals
MMTV (mouse mammary tumor virus)	Glucocorticoids
β -Interferon	poly(rI)X, poly(rc)
Adenovirus 5 E2	Ela
c-jun	Phorbol Ester (TPA), H ₂ O ₂
Collagenase	Phorbol Ester (TPA)
Stromelysin	Phorbol Ester (TPA), IL-1
SV40	Phorbol Ester (TPA)
Murine MX Gene	Interferon, Newcastle Disease Virus
GRP78 Gene	A23187
α -2-Macroglobulin	IL-6
Vimentin	Serum
MHC Class I Gene H-2kB	Interferon
HSP70	Ela, SV40 Large T Antigen
Proliferin	Phorbol Ester-TPA
Tumor Necrosis Factor	FMA

Element	Inducer
Thyroid Stimulating Hormone α Gene	Thyroid Hormone
Insulin E Box	Glucose

Binding Moieties

[00206] In some embodiments of the invention, the target cell or pathogen(s) of interest, or nucleic acids from the target cell or pathogen, may be captured, immobilized and/or labeled by binding to one or more binding moieties. A variety of binding moieties are known in the art, including but not limited to oligonucleotides, nucleic acids, aptamers, antibodies, antibody fragments, chimeric antibodies, single-chain antibodies, ligands, binding proteins, lectins, receptor proteins, inhibitors, substrates, *etc.* Any such known binding moiety may be used in the claimed methods. Exemplary binding moieties - antibodies and aptamers - are discussed in further detail below. Methods for design and production of oligonucleotide binding moieties, *e.g.* for hybridization to a pathogen nucleic acid and/or oligonucleotide tag, are known in the art and are similar to the methods for primer production discussed above. Binding moieties may be purchased from a wide variety of commercial sources, or may be generated using methods well known in the art (*e.g.* U.S. Patent Nos. 5,270,163; 5,567,588; 5,670,637; 5,696,249; 5,843,653; Harlowe and Lane, Antibodies: A Laboratory Manual, Cold Spring Harbor Press, Cold Spring Harbor, NY, 1988).

Antibodies

[00207] Methods for preparing and characterizing antibodies are well known in the art (see, *e.g.*, Harlow and Lane, 1988). Antibodies of use may be monoclonal or polyclonal. In preferred embodiments, monoclonal antibodies are used. Antibodies against a wide variety of antigens are available from commercial sources. Alternatively, antibodies against a novel target may be prepared as disclosed herein.

[00208] Antibodies are prepared by immunizing an animal with an immunogen (antigen) and collecting antisera from the immunized animal. A wide range of animal species can be used for the production of antisera. Typical animals used for production of polyclonal antibodies include, rabbits, mice, rats, hamsters, pigs or horses. Because of the relatively large blood volume of

rabbits, a rabbit is a preferred choice for production of polyclonal antibodies, while mice are preferred for monoclonal antibody production.

[00209] Antibodies, both polyclonal and monoclonal, may be prepared using conventional immunization techniques, generally known in the art. A composition containing antigenic epitopes can be used to immunize one or more experimental animals, such as a rabbit or mouse, which will then produce specific antibodies against the antigens of interest. Polyclonal antisera may be obtained, after allowing time for antibody generation, simply by bleeding the animal and preparing serum samples from the whole blood.

[00210] As is well known in the art, a given composition may vary in its immunogenicity. It is often necessary to boost the host immune system, as may be achieved by coupling a peptide or polypeptide immunogen to a carrier. Exemplary carriers are keyhole limpet hemocyanin (KLH) and bovine serum albumin (BSA). Other albumins such as ovalbumin, mouse serum albumin or rabbit serum albumin also can be used as carriers. Techniques for conjugating a polypeptide to a carrier protein are well known in the art and include use of cross-linking reagents such as glutaraldehyde, *m*-maleimidobenzoyl-N-hydroxysuccinimide ester, carbodiimide and bis-biazotized benzidine. The immunogenicity of a particular immunogen composition may also be enhanced by the use of non-specific stimulators of the immune response, known as adjuvants. Exemplary adjuvants include complete Freund's adjuvant (a non-specific stimulator of the immune response containing killed *Mycobacterium tuberculosis*), incomplete Freund's adjuvant and aluminum hydroxide adjuvant.

[00211] The amount of immunogen composition used in the production of polyclonal antibodies varies upon the nature of the immunogen as well as the animal used for immunization. A variety of routes can be used to administer the immunogen (subcutaneous, intramuscular, intradermal, intravenous and intraperitoneal). Booster injections also may be given. The process of boosting and titering is repeated until a suitable titer is achieved. When a desired level of immunogenicity is obtained, the immunized animal can be bled and the serum isolated and stored, and/or the animal can be used to generate monoclonal antibodies.

[00212] Monoclonal antibodies may be readily prepared through use of well-known techniques, such as those exemplified in U.S. Patent 4,196,26. Typically, this involves immunizing a suitable animal with a selected immunogen composition. Following immunization, somatic cells

with the potential for producing antibodies, specifically B-lymphocytes (B-cells), are selected for use in the mAb generating protocol. These cells may be obtained from biopsied spleens, tonsils or lymph nodes, or from a peripheral blood sample. Spleen cells and peripheral blood cells are preferred, the former because they are a rich source of antibody-producing cells that are in the dividing plasmablast stage, and the latter because peripheral blood is easily accessible. Often, a panel of animals will have been immunized and the spleen of the animal with the highest antibody titer will be removed and the spleen lymphocytes obtained by homogenizing the spleen with a syringe. Typically, a spleen from an immunized mouse contains approximately 5×10^7 to 2×10^8 lymphocytes.

[00213] The antibody-producing B lymphocytes from the immunized animal are then fused with cells of an immortal myeloma cell. Any one of a number of myeloma cells may be used, as are known to those of skill in the art (Goding, *In: Monoclonal Antibodies: Principles and Practice*, 2d ed., Academic Press, Orlando, Fla., pp. 60-61, and 71-74, 1986; Campbell, *In: Monoclonal Antibody Technology, Laboratory Techniques in Biochemistry and Molecular Biology*, Burden and Von Knippenberg, Eds., Vol. 13:75-83, Elsevier, Amsterdam, 1984). For example, where the immunized animal is a mouse, one may use P3-X63/Ag8, P3-X63-Ag8.653, NS1/1.Ag 4 1, Sp210-Ag14, FO, NSO/U, MPC-11, MPC11-X45-GTG 1.7 and S194/5XX0 Bul; for rats, one may use R210.RCY3, Y3-Ag 1.2.3, IR983F and 4B210; and U-266, GM1500-GRG2, LICR-LON-HMy2 and UC729-6 are all useful in connection with cell fusions.

[00214] Methods for generating hybrids of antibody-producing spleen or lymph node cells and myeloma cells usually comprise mixing somatic cells with myeloma cells in a 2:1 ratio, though the ratio may vary from about 20:1 to about 1:1, respectively, in the presence of an agent or agents (chemical or electrical) that promote the fusion of cell membranes. Fusion methods using Sendai virus (Kohler and Milstein, *Nature*, 256:495-497, 1975; *Eur. J. Immunol.*, 6: 511-519, 1976), and those using polyethylene glycol (PEG), such as 37% (v/v) PEG, have been disclosed by Gefter *et al.*, (*Somatic Cell Genet.*, 3: 231-236, 1977). The use of electrically induced fusion methods is also appropriate (Goding, 1986).

[00215] Fusion procedures usually produce viable hybrids at low frequencies, around 1×10^{-6} to 1×10^{-8} . However, fused hybrids may be differentiated from the parental, unfused cells by culturing in a selective medium. The selective medium generally contains an agent that blocks

the *de novo* synthesis of nucleotides in the tissue culture media. Exemplary and preferred agents are aminopterin, methotrexate, and azaserine. Where aminopterin or methotrexate is used, the media is supplemented with hypoxanthine and thymidine as a source of nucleotides (HAT medium). Where azaserine is used, the media is supplemented with hypoxanthine. A preferred selection medium is HAT. The only cells that can survive in the selective media are those hybrids formed from myeloma and B-cells.

[00216] Typically, selection of hybridomas is performed by culturing the cells by single-clone dilution in microtiter plates, followed by testing the individual clonal supernatants (after about two to three wk) for the desired reactivity. The selected hybridomas may then be serially diluted and cloned into individual antibody-producing cell lines, which clones can be propagated indefinitely to provide mAbs.

Aptamers

[00217] In certain embodiments of the invention, the binding moieties to be used may comprise aptamers. Methods of constructing and determining the binding characteristics of aptamers are well known in the art. For example, such techniques are disclosed in Lorsch and Szostak (In: Combinatorial Libraries: Synthesis, Screening and Application Potential, R. Cortese, ed., Walter de Gruyter Publishing Co., New York, pp. 69-86, 1996) and in U.S. Patent Nos. 5,582,981, 5,595,877 and 5,637,459. Aptamers may be comprised of DNA or RNA. Alternatively, once a given aptamer sequence has been identified, modified oligomers of the same sequence may be prepared to provide enhanced stability to nucleases. Any of the hydroxyl groups ordinarily present in oligonucleotides may be replaced by phosphonate groups, phosphate groups, protected by a standard protecting group, or activated to prepare additional linkages to other nucleotides, or may be conjugated to solid supports. The 5' terminal OH is conventionally free but may be phosphorylated. Hydroxyl group substituents at the 3' terminus may also be phosphorylated. The hydroxyls may be derivatized by standard protecting groups. One or more phosphodiester linkages may be replaced by alternative linking groups. These alternative linking groups include exemplary embodiments wherein P(O)O is replaced by P(O)S, P(O)NR₂, P(O)R, P(O)OR', CO, or CNR₂, wherein R is H or alkyl (1-20C) and R' is alkyl (1-20C); in addition, this group may be attached to adjacent nucleotides through O or S. Not all linkages in an oligomer need to be identical.

[00218] In preferred embodiments, the starting pool of oligonucleotides (referred to as nucleic acid ligands) used to prepare aptamers will contain a randomized sequence portion flanked by primer sequences that permit the amplification of nucleic acid ligands found to bind to a selected target. Both the randomized portion and the primer hybridization regions of the initial nucleic acid ligand population may be constructed using conventional solid phase techniques. Such techniques are well known in the art (*e.g.*, Froehler, *et al.*, *Tet Lett.* 27:5575-5578, 1986a; *Nucleic Acids Research*, 14:5399-5467, 1986b; *Nucleosides and Nucleotides*, 6:287-291, 1987; *Nucleic Acids Research*, 16:4831-4839, 1988). For synthesis of the randomized regions, mixtures of nucleotides at the positions where randomization is desired are added during synthesis.

[00219] A preferred method of selecting for aptamers of specific binding activity involves use of the SELEX process, disclosed for example in U.S. Pat. No. 5,475,096 and U.S. Pat. No. 5,270,163. SELEX involves selection from a mixture of candidate nucleic acid ligands and step-wise iterations of binding, partitioning and amplification, using the same general selection scheme, to achieve any desired criterion of binding affinity and selectivity. Starting from a mixture of nucleic acid ligands, the method includes: Contacting the mixture with the target under conditions favorable for binding. Partitioning unbound nucleic acid ligands from those nucleic acid ligands that have bound specifically to target analyte. Dissociating the nucleic acid ligand-analyte complexes. Amplifying the nucleic acid ligands dissociated from the nucleic acid ligand-analyte complexes to yield a mixture of nucleic acid ligands that preferentially bind to the analyte. Reiterating the steps of binding, partitioning, dissociating and amplifying through as many cycles as desired to yield highly specific aptamers that bind with high affinity to the target analyte.

Labels

[00220] In certain embodiments of the invention, one or more labels may be attached to a binding moiety, probe, primer or other molecule. A number of different labels may be used, such as fluorophores, chromophores, radioisotopes, enzymatic tags, antibodies, bioluminescent, electroluminescent, phosphorescent, affinity labels, nanoparticles, metal nanoparticles, gold nanoparticles, silver nanoparticles, magnetic particles, spin labels or any other type of label known in the art.

[00221] Non-limiting examples of affinity labels include an antibody, an antibody fragment, a receptor protein, a hormone, biotin, DNP, and any polypeptide/protein molecule that binds to an affinity label.

[00222] Non-limiting examples of enzymatic tags include urease, alkaline phosphatase or peroxidase. Colorimetric indicator substrates can be employed with such enzymes to provide a detection means visible to the human eye or spectrophotometrically.

[00223] Non-limiting examples of photodetectable labels include Alexa 350, Alexa 430, AMCA, aminoacridine, BODIPY 630/650, BODIPY 650/665, BODIPY-FL, BODIPY-R6G, BODIPY-TMR, BODIPY-TRX, 5-carboxy-4',5'-dichloro-2',7'-dimethoxy fluorescein, 5-carboxy-2',4',5',7'-tetrachlorofluorescein, 5-carboxyfluorescein, 5-carboxyrhodamine, 6-carboxyrhodamine, 6-carboxytetramethyl amino, Cascade Blue, Cy2, Cy3, Cy5,6-FAM, dansyl chloride, Fluorescein, HEX, 6-JOE, NBD (7-nitrobenz-2-oxa-1,3-diazole), Oregon Green 488, Oregon Green 500, Oregon Green 514, Pacific Blue, phthalic acid, terephthalic acid, isophthalic acid, cresyl fast violet, cresyl blue violet, brilliant cresyl blue, para-aminobenzoic acid, erythrosine, phthalocyanines, azomethines, cyanines, xanthenes, succinylfluoresceins, rare earth metal cryptates, europium trisbipyridine diamine, a europium cryptate or chelate, diamine, dicyanins, La Jolla blue dye, allophycocyanin, allococyanin B, phycocyanin C, phycocyanin R, thiamine, phycoerythrocyanin, phycoerythrin R, REG, Rhodamine Green, rhodamine isothiocyanate, Rhodamine Red, ROX, TAMRA, TET, TRIT (tetramethyl rhodamine isothiol), Tetramethylrhodamine, and Texas Red. These and other luminescent labels may be obtained from commercial sources such as Molecular Probes (Eugene, OR).

[00224] In other embodiments of the invention, labels of use may comprise metal nanoparticles. Methods of preparing nanoparticles are known. (*See e.g.*, U.S. Patent Nos. 6,054,495; 6,127,120; 6,149,868; Lee and Meisel, *J. Phys. Chem.* 86:3391-3395, 1982.) Nanoparticles may also be obtained from commercial sources (*e.g.*, Nanoprobes Inc., Yaphank, NY; Polysciences, Inc., Warrington, PA). Modified nanoparticles are available commercially, such as Nanogold® nanoparticles from Nanoprobes, Inc. (Yaphank, NY).

[00225] In some embodiments of the invention, proteins may be labeled using side-chain specific and/or selective reagents. Such reagents and methods are known in the art. Non-limiting exemplary reagents that may be used include acetic anhydride (lysine, cysteine, serine

and tyrosine); trinitrobenzenesulfonate (lysine); carbodiimides (glutamate, aspartate); phenylglyoxal (arginine); 2,3-butanedione (arginine); pyridoxal phosphate (lysine); *p*-chloromercuribenzoate (cysteine); 5,5'-dithiobis(2-nitro-benzoic acid) (cysteine); diethylpyrocarbonate (lysine, histidine); N-bromosuccinimide (tryptophan) and tetranitromethane (cysteine, tyrosine). Various methods for attaching labels to nucleic acids and/or oligonucleotides are known in the art and may be used. For example, water-soluble carbodiimides may be used to cross-link the phosphate groups of nucleic acids or oligonucleotides to various labels. Amino or sulfhydryl modified oligonucleotides or nucleic acids may be attached to labels using known bifunctional crosslinking reagents (Running *et al.*, *BioTechniques* 8:276-277, 1990; Newton *et al.*, *Nucleic Acids Res.* 21:1155-62, 1993).

[00226] In alternative embodiments of the invention, various cross-linking reagents known in the art, such as homo-bifunctional, hetero-bifunctional and/or photoactivatable cross-linking reagents may be used. Non-limiting examples of such reagents include bisimidates; 1,5-difluoro-2,4-(dinitrobenzene); N-hydroxysuccinimide ester of suberic acid; disuccinimidyl tartarate; dimethyl-3,3'-dithio-bispropionimide; N-succinimidyl-3-(2-pyridyldithio)propionate; 4-(bromoaminoethyl)-2-nitrophenylazide; and 4-azidoglyoxal. Such reagents may be modified to attach various types of labels, such as fluorescent labels. The skilled artisan will realize that such cross-linking reagents are not limited to use with proteins, but may also be used with other types of molecules.

Methods of Immobilization

[00227] In various embodiments of the invention, binding moieties, capture probes or analytes of interest may be attached to a surface by covalent or non-covalent interaction. One means for promoting such attachments involves the use of chemical or photo-activated cross-linking reagents. Such reagents are well known in the art.

[00228] Homobifunctional reagents that carry two identical functional groups are highly efficient in inducing cross-linking. Heterobifunctional reagents contain two different functional groups. By taking advantage of the differential reactivities of the two different functional groups, cross-linking can be controlled both selectively and sequentially. The bifunctional cross-linking reagents can be divided according to the specificity of their functional groups, *e.g.*, amino, sulfhydryl, guanidino, indole, carboxyl specific groups. Of these, reagents directed to

free amino groups have become especially popular because of their commercial availability, ease of synthesis and the mild reaction conditions under which they can be applied. A majority of heterobifunctional cross-linking reagents contains a primary amine-reactive group and a thiol-reactive group.

[00229] Exemplary methods for cross-linking molecules are disclosed in U.S. Patent 5,603,872 and U.S. Patent 5,401,511. Various ligands can be covalently bound to surfaces through the cross-linking of amine residues. Amine residues may be introduced onto a surface through the use of aminosilane, for example. Coating with aminosilane provides an active functional residue, a primary amine, on the surface for cross-linking purposes. In another exemplary embodiment, the surface may be coated with streptavidin or avidin with the subsequent attachment of a biotinylated molecule, such as an antibody or analyte. To form covalent conjugates of ligands and surfaces, various cross-linking reagents have been used, including glutaraldehyde (GAD), bifunctional oxirane (OXR), ethylene glycol diglycidyl ether (EGDE), and a water soluble carbodiimide, preferably 1-ethyl-3-(3-dimethylaminopropyl) carbodiimide (EDC).

[00230] In another non-limiting example, heterobifunctional cross-linking reagents and methods of using the cross-linking reagents are disclosed in U.S. Patent Serial No. 5,889,155. The cross-linking reagents combine, for example, a nucleophilic hydrazide residue with an electrophilic maleimide residue, allowing coupling in one example, of aldehydes to free thiols. The cross-linking reagent used can be designed to cross-link various functional groups. In various embodiments, the target to be analyzed may be attached to a solid surface (or immobilized). Immobilization may be achieved by a variety of methods involving either non-covalent or covalent attachment. In an exemplary embodiment, immobilization may be achieved by coating a surface with streptavidin or avidin and the subsequent attachment of a biotinylated molecule (Holmstrom *et al.*, *Anal. Biochem.* 209:278-283, 1993). Immobilization may also occur by coating a silicon, glass or other surface with poly-L-Lys (lysine), followed by covalent attachment of either amino- or sulfhydryl-modified molecule using bifunctional crosslinking reagents (Running *et al.*, *BioTechniques* 8:276-277, 1990; Newton *et al.*, *Nucleic Acids Res.* 21:1155-62, 1993).

[00231] Immobilization of nucleic acids or oligonucleotides may take place by direct covalent attachment of 5'-phosphorylated nucleic acids to chemically modified surfaces (Rasmussen *et al.*, *Anal. Biochem.* 198:138-142, 1991). The covalent bond between the nucleic acid and the surface is formed by condensation with a water-soluble carbodiimide. This method facilitates a predominantly 5'-attachment of the nucleic acids via their 5'-phosphates. DNA is commonly bound to glass by first silanizing the glass surface, then activating with carbodiimide or glutaraldehyde. Alternative procedures may use reagents such as 3-glycidoxypropyltrimethoxysilane (GOP) or aminopropyltrimethoxysilane (APTS) with DNA linked *via* amino linkers incorporated either at the 3' or 5' end of the molecule. DNA may be bound directly to membrane surfaces using ultraviolet radiation. Other non-limiting examples of immobilization techniques for nucleic acids are disclosed in U.S. Patent Nos. 5,610,287, 5,776,674 and 6,225,068.

[00232] The type of surface to be used for immobilization is not limiting. In various embodiments, the immobilization surface may be magnetic beads, non-magnetic beads, a planar surface, or any other conformation of solid surface comprising almost any material. Non-limiting examples of surfaces that may be used include glass, silica, silicate, PDMS, silver or other metal coated surfaces, nitrocellulose, nylon, activated quartz, activated glass, polyvinylidene difluoride (PVDF), polystyrene, polyacrylamide, other polymers such as poly(vinyl chloride), poly(methyl methacrylate) or poly(dimethyl siloxane), and photopolymers which contain photoreactive species such as nitrenes, carbenes and ketyl radicals capable of forming covalent links with various molecules (See U.S. Pat. Nos. 5,405,766 and 5,986,076).

Statistical Signal Processing

[00233] In certain embodiments of the invention, statistical signal processing may be used to deconvolute a complex signal into its individual components. For example, some embodiments may involve sequencing of pathogen nucleic acids, using a mixture of nucleotides that are distinguishably labeled with different fluorophores. Nucleic acid sequence analysis may be used to distinguish different strains of pathogens that differ by a single base-pair in their nucleic acid sequences. In other embodiments, the presence of different target cells or pathogens in a sample may be simultaneously assayed using distinguishably labeled probes that bind specifically to

different targets. Such methods may benefit from the use of signal processing techniques disclosed herein.

[00234] The signal processing techniques are generally applicable where a number of otherwise identical reactions or processes occur simultaneously, with variable temporal offset. This may occur, for example, where multiple copies of a DNA template are being simultaneously replicated. Although in preferred embodiments, all copies of a given template will be subject to a coordinated initiation of replication, random variations in the polymerization process will rapidly result in a distribution of reaction rates, with some complementary strands synthesized earlier and others synthesized later. The resulting temporal offset in signal detection will soon result in a highly convoluted signal that may preferably be deconvoluted before further analysis.

[00235] For a fixed signature signal $s(t)$ of duration T seconds, i.e.,

$$s(t) \neq 0 \quad \text{for} \quad 0 \leq t \leq T \quad (27)$$

and

$$s(t) = 0 \quad \text{for} \quad t < 0, t > T \quad (28)$$

the random superposition of N such signatures immersed in noise may be observed. The observed signal may be described by

$$y(t) = \sum_{n=1}^N s(t - d_n) + v(t), \quad (29)$$

where d_n represents the random delay (time shift) for the n th ($n = 1, 2, \dots, N$) signature sequence and where $v(t)$ represents the noise process. It is assumed that the observed signal starts at time $t=0$, so that all the delays are non-negative (i.e., $d_n \geq 0$).

[00236] In practice, continuous signals are rarely measured. Rather what are measured are the sampled values of the signal, obtained from sampling at a certain rate. With a sampling rate of R samples per second, the signature signal may be represented by the following sequence of length $L = RT + 1$

$$s_i = s(i/R), \quad i = 0, 1, \dots, RT. \quad (30)$$

[00237] In this case, the sampled observation signal $y_i = y(i/R)$ is simply

$$y_i = \sum_{n=1}^N s_{i-k_n} + v_i, \quad (31)$$

where $v_i = v(i/R)$ represents the samples of the noise and where k_n represents the delay via the formula

$$k_n = \lfloor Rd_n \rfloor. \quad (32)$$

[00238] Equation 31 assumes that the sequence s_i is zero for $i \leq 0$. An important condition for the present analysis is that N is very large. In this case it is reasonable to consider a distribution for the delays d_n , or k_n . If N_j denotes the number of signature sequences that begin at time j , i.e., the number of n such that $k_n = j$, Equation 31 may be rewritten as

$$y_i = \sum_{j=0}^D N_j s_{i-j} + v_i, \quad (33)$$

where D represents the total duration of the delays. In other words, the delays j extend from $j=0$ to $j=D$. Note, moreover, that

$$\sum_{j=0}^D N_j = N \quad (34)$$

and that the total duration of the observed signal is

$$D + RT + 1. \quad (35)$$

It is also possible to write the “convolution” in Equation 33 as

$$y_i = \sum_{j=0}^{RT} N_{i-j} s_j + v_i. \quad (36)$$

[00239] It is now possible to resolve the following problem. Given the observations sequence y_i , satisfying Equation 33, or equivalently Equation 36, determine the unknown signature sequence s_i . A standard assumption for the noise process v_i is that it is zero-mean, Gaussian and white, i.e., uncorrelated in time---although other types of noise models can also be dealt with, e.g., zero-mean Gaussian noise with a certain power spectral density function.

[00240] If the N_j in Equation 33 or Equation 36 are assumed to be known then we are simply confronted with an overdetermined system of linear equations in the unknowns s_i . To see this more explicitly, it is useful to rewrite Equation 33 in the following form

$$\begin{bmatrix} y_0 \\ y_1 \\ \vdots \\ y_{D+RT-1} \\ y_{D+RT} \end{bmatrix} = \begin{bmatrix} N_0 & & & & \\ N_1 & N_0 & & & \\ \vdots & N_1 & \ddots & & \\ N_D & \vdots & \ddots & N_0 & \\ & N_D & \vdots & N_1 & \\ & & \ddots & \vdots & \\ & & & N_D & \end{bmatrix} \begin{bmatrix} s_0 \\ s_1 \\ \vdots \\ s_{RT-1} \\ s_{RT} \end{bmatrix} + \begin{bmatrix} v_0 \\ v_1 \\ \vdots \\ v_{D+RT-1} \\ v_{D+RT} \end{bmatrix}. \quad (37)$$

[00241] With the N_j known, the coefficient matrix in Equation 37 is known. Therefore the unknown vector of s_i 's can be readily computed via standard methods such as least-squares. The problem is that the N_j are not known. All that is observed is the sequence y_i . Therefore we are confronted with an equation where all the quantities on the right-hand-side (the N_j , s_i and v_i) are unknown. A natural question is whether in principle the desired s_i may be identified from Equation 37.

[00242] If it is assumed that the noise vector of v_i 's is negligible, then Equation 37 is a system of $D + RT + 1$ equations (the number of observations) in $D + RT + 2$ unknowns ($D + 1$ unknowns for the N_j and $RT + 1$ unknowns for the s_i). Therefore, even in the noiseless case, it appears that there is an identifiability problem for there are more unknowns than equations. Of course, it is possible to use the equation $\sum_{j=0}^D N_j = N$ to get the number of equations and unknowns to match. However, with some very reasonable statistical assumptions it is possible to circumvent the identifiability problem altogether.

Statistical Assumptions: Exploiting Large N

[00243] A distinguishing feature of sequencing problems is that the number of DNA molecules, and hence signature sequences, N is extremely large. Therefore if something is known about the statistics of the delay distribution then it is possible to "estimate" the values of the N_j , and thereby the coefficient matrix in Equation 37. The statistics of the delay distribution is a *macroscopic* quantity, and so it is reasonable to assume that it is known. Moreover, being a

macroscopic quantity, it is also reasonable to assume that it may be controlled using an appropriate system design. This statistical knowledge can be used to estimate the N_j .

[00244] Uniform delay distribution: Assume that the delay distribution is uniform over D , the duration of the delays. In other words, the signature sequences are equally likely to begin anywhere in the interval $[0, D]$. This assumption is true in many applications and the sequencing system may be designed to exhibit a uniform delay distribution over D .

[00245] Using properties of the binomial distribution, each of the N_j will be random variables with mean and variance

$$\mu_N = EN_j = N/D \quad \text{and} \quad \sigma_N^2 = E(N_j - N/D)^2 = (1 - 1/D)N/D \quad (38)$$

where E denotes expectation. It can also be shown that the random variables N_j have cross-covariance:

$$C_{N_i N_j} = E(N_i - N/D)(N_j - N/D) = -N/D^2. \quad (39)$$

[00246] Equation 38 shows that as N grows larger the mean N/D becomes a better and better estimate of the actual value N_j . The ratio of the standard deviation of N_j to its mean is given by

$$\frac{\sigma_N}{\mu_N} = \sqrt{\frac{D-1}{N}}, \quad (40)$$

which goes to zero as N goes to infinity, so that the estimate becomes more and more reliable with larger sample size. If we define the random variable $\tilde{N}_j = N_j - N/D$, Equation 37 may be rewritten as:

$$\begin{bmatrix} y_0 \\ y_1 \\ \vdots \\ y_{D+RT-1} \\ y_{D+RT} \end{bmatrix} = \frac{N}{D} \begin{bmatrix} 1 & & & & \\ 1 & 1 & & & \\ \vdots & 1 & \ddots & & \\ 1 & \vdots & \ddots & 1 & \\ & 1 & \vdots & 1 & \\ & & \ddots & \vdots & 1 \\ & & & 1 & \end{bmatrix} \begin{bmatrix} s_0 \\ s_1 \\ \vdots \\ s_{RT-1} \\ s_{RT} \end{bmatrix} + \begin{bmatrix} \tilde{N}_0 & & & & \\ \tilde{N}_1 & \tilde{N}_0 & & & \\ \vdots & \tilde{N}_1 & \ddots & & \\ \tilde{N}_D & \vdots & \ddots & \tilde{N}_0 & \\ & \tilde{N}_D & \vdots & \tilde{N}_1 & \\ & & \ddots & \vdots & \\ & & & \tilde{N}_D & \end{bmatrix} \begin{bmatrix} s_0 \\ s_1 \\ \vdots \\ s_{RT-1} \\ s_{RT} \end{bmatrix} + \begin{bmatrix} v_0 \\ v_1 \\ \vdots \\ v_{D+RT-1} \\ v_{D+RT} \end{bmatrix}. \quad (41)$$

[00247] In Equation 41, the matrix coefficient in the first term is known. Although the second matrix coefficient is unknown its “energy” is less by a factor of N . To make this more precise, defining the last two terms in Equation 41 as an “equivalent” noise

$$\begin{bmatrix} w_0 \\ w_1 \\ \vdots \\ w_{D+RT-1} \\ w_{D+RT} \end{bmatrix} = \begin{bmatrix} \tilde{N}_0 & & & & \\ \tilde{N}_1 & \tilde{N}_0 & & & \\ \vdots & \tilde{N}_1 & \ddots & & \\ \tilde{N}_D & \vdots & \ddots & \tilde{N}_0 & \\ & \tilde{N}_D & \vdots & \tilde{N}_1 & \\ & & \ddots & \vdots & \\ & & & \tilde{N}_D & \end{bmatrix} \begin{bmatrix} s_0 \\ s_1 \\ \vdots \\ s_{RT-1} \\ s_{RT} \end{bmatrix} + \begin{bmatrix} v_0 \\ v_1 \\ \vdots \\ v_{D+RT-1} \\ v_{D+RT} \end{bmatrix}, \quad (42)$$

[00248] Using Equation 38 and Equation 39 it is straightforward to compute the covariance matrix of the equivalent noise. If the off-diagonal terms are ignored compared to the diagonal ones (from Equations 38 and 39 σ_N^2 is larger than $C_{N_i N_j}$ by a factor of D), then the covariance matrix can be written as

$$R_w = \begin{bmatrix} \sigma_v^2 + \frac{NP_s}{DRT} & & & & \\ & \sigma_v^2 + \frac{2NP_s}{DRT} & & & \\ & & \ddots & & \\ & & & \sigma_v^2 + \frac{NP_s}{D} & \\ & & & & \ddots \\ & & & & & \sigma_v^2 + \frac{NP_s}{D} & \\ & & & & & & \ddots \\ & & & & & & & \sigma_v^2 + \frac{2NP_s}{DRT} \\ & & & & & & & & \sigma_v^2 + \frac{NP_s}{DRT} \end{bmatrix}$$

for $D > RT$ and

$$R_w = \begin{bmatrix} \sigma_v^2 + \frac{NP_s}{DRT} & & & & \\ & \sigma_v^2 + \frac{2NP_s}{NRT} & & & \\ & & \ddots & & \\ & & & \sigma_v^2 + \frac{N(D+RT)}{2DRT} & \\ & & & & \ddots \\ & & & & & \sigma_v^2 + \frac{2NP_s}{DRT} \\ & & & & & & \sigma_v^2 + \frac{NP_s}{DRT} \end{bmatrix}$$

for $D < RT$, where the noise variance is defined as $E v_i v_j = \sigma_v^2 \delta_{ij}$ and the signature signal energy is defined as

$$P_s = \sum_{i=0}^{RT} s_i^2. \quad (43)$$

[00249] An important quantity is the “equivalent” signal-to-noise-ratio (SNR), which can be computed to be

$$SNR = \frac{SNR_{perfect}}{1 + \frac{D}{N} SNR_{perfect}}, \quad (44)$$

where

$$SNR_{perfect} = \frac{N^2 P_s}{D(D+RT)\sigma_v^2}, \quad (45)$$

is the SNR when we have *exact* knowledge of the N_j . As N goes to infinity, SNR approaches $SNR_{perfect}$. In other words, in the limit of large N , the system behaves as if the values of the N_j are known. Thus, the macroscopic statistical knowledge allows circumvention of the identifiability problem.

[00250] The Wiener solution: Now that all the relevant covariance matrices have been computed, it is straightforward to find the least-mean-squares estimate of the signature sequence. The solution is referred to as the *Wiener solution* and is given by

$$\begin{bmatrix} \hat{s}_0 \\ \hat{s}_1 \\ \vdots \\ \hat{s}_{RT-1} \\ \hat{s}_{RT} \end{bmatrix} = \frac{NP_s}{DRT} \Theta^* (R_w + \frac{N^2 P_s}{D^2 RT} \Theta \Theta^*)^{-1} \begin{bmatrix} y_0 \\ y_1 \\ \vdots \\ y_{D+RT-1} \\ y_{D+RT} \end{bmatrix}, \quad (46)$$

where the $(D + RT + 1) \times (RT + 1)$ Toeplitz matrix Θ from Equation 41 is defined as

$$\Theta = \begin{bmatrix} 1 & & & & \\ 1 & 1 & & & \\ \vdots & 1 & \ddots & & \\ 1 & \vdots & \ddots & 1 & \\ & 1 & \vdots & 1 & \\ & & \ddots & \vdots & \\ & & & & 1 \end{bmatrix}. \quad (47)$$

[00251] The Wiener solution shown in Equation 46 requires computing the inverse of a $(D + RT + 1) \times (D + RT + 1)$ matrix. Due to the Toeplitz structure this can be done efficiently and in a numerically stable way. Exemplary resolutions of the inverse matrix computation using the Wiener solution are provided below in the Examples section.

EXAMPLES

Example 1: BRC Assay

Sample Preparation

[00252] Total RNA extracts may be obtained from blood, tissues or cell lines using commercially available kits (*e.g.*, Ambion, Austin, TX; Qiagen, Valencia, CA; Promega, Madison, WI). cDNA may be synthesized using a SuperScript™ or other commercial kit (Invitrogen Life Technologies, Austin, TX). Where preferred, polyadenylated mRNA may be purified by oligo(dT) column chromatography or other known methods. Genomic DNA may be prepared by standard techniques (*e.g.*, Sambrook *et al.*, 1989).

[00253] In an exemplary embodiment, first strand cDNA synthesis employed an RNA/primer mixture containing 5 μ l total RNA and 1 μ l of 0.5 μ g/ μ l oligo(dT) random primer or gene specific primer, incubated at 70°C for 10 min and then placed on ice for at least 1 min. A reaction mixture containing 2 μ l 10X buffer (0.1 M Tris-Acetate pH 7.75, 5 mM EDTA, 50 mM Mg-acetate, 2 mM kinase free dNTP and 0.1 M dithiothreitol) in which dATP was replaced with α -thio dATP was added to the RNA/primer mixture, mixed gently, collected by brief centrifugation and then incubated at 42°C for 5 min. After addition of 200 U of SuperScript II reverse transcriptase, the tube was incubated at 40°C for 15 min. The reaction was terminated by heating at 70°C for 15 min and then chilling on ice. The dNTP used in cDNA synthesis was kinase free. In preferred embodiments dATP is replaced with alpha-thio dATP or analogs that are not good substrates for luciferase.

[00254] An aliquot of synthesized cDNA was added to 50 μ l of reaction mixture (see Ronaghi *et al.*, *Anal. Biochem.* 242:84-89, 1996 with modifications) containing 250 ng luciferase (Promega, Madison, WI), 50 mU ATP sulfurylase (Sigma Chemical Co., St. Louis, MO), 2 mM dithiothreitol, 100 mM Tris-Acetate pH 7.75, 0.5 mM EDTA, 0.5 mg BSA, 0.2 mg polyvinylpyrrolidone (M_r 360.000), 10 μ g D-luciferin (Biothema, Dalaro, Sweden), 5 mM magnesium acetate and 0.01 to 10 attomole purified pyrophosphate or ATP. The addition of very low amounts of pyrophosphate or ATP (or analogs) was found to decrease background light emission from the reaction mixture. Although the precise mechanism is unknown, BRC performed without adding small amounts of ATP or P_{pi} consistently exhibited background luminescence that precluded accurate measurement of pathogen nucleic acids present in amounts of about a femtomole or lower. Inorganic pyrophosphate present in the cDNA sample as a result of polymerase mediated dNTP incorporation was converted to ATP by sulfurylase. The ATP was used to generate light in a luciferin/luciferase reaction.

[00255] The generated light intensity over a time interval may be used to calculate the number of mRNAs converted to cDNA by reverse transcriptase. In this exemplary process, the total amount of polyadenylated RNA present in the sample was determined, using oligo(dT) random primers. The presence of specific pathogen nucleic acids may be determined using sequence specific primers, as detailed below.

Synthesis and Purification of Sequence Specific Oligonucleotide Primers

[00256] The following oligonucleotides were synthesized and HPLC purified by MWG Biotech (High Points, NC).

B-MBPup

Biotin-5'-CGGCGATAAAGGCTATAACGG-3' (SEQ ID NO:1)

MBPup

5'-CGGCGATAAAGGCTATAACGG-3' (SEQ ID NO:2)

B-MBPR1

Biotin-5'-CTGGAACGCTTTGTCCGGGG-3' (SEQ ID NO:3)

MBPR1

5'-CTGGAACGCTTTGTCCGGGG-3' (SEQ ID NO:4)

oligo-loop

5'TTTTTTTTTTTTTTTTTTTTGTCTGGAATTCGTCAGACTGGCCGTCGTTT

TACAACGGAACGGCAGCAAAATGTTGC-3' (SEQ ID NO:5)

Template Preparation

[00257] Biotinylated PCR products were prepared from bacterial extracts containing pMAL vector (New England Biolabs, Beverly, MA) (Pourmand et al. 1998, Autoimmunity 28; 225-233) by standard techniques, using MBPup and biotinylated B-MBPR1 or MBPR1 and biotinylated B-MBPup as PCR primers. The PCR products were immobilized onto streptavidin-coated superparamagnetic beads (Dynabeads™ M280-Streptavidin, Dynal A.S., Oslo, Norway). Single-stranded DNA was obtained by incubating the immobilized PCR product in 0.10 M NaOH for 3 min to separate strands and then removing the supernatant.

Strand Extension

[00258] The immobilized single stranded PCR product was resuspended in annealing buffer (10 mM Tris-acetate pH 7.75, 2 mM Mg-acetate) and placed into wells of a microtiter plate. Five pmol of the BRC primers MBP-up (SEQ ID NO:2) or MBPR1 (SEQ ID NO:4) were added to the immobilized strand obtained from the PCR reaction (depending on what set of biotinylated PCR primers was used). Hybridization of the template and primers was performed by incubation at 95°C for 3 min, 55°C for 5 min and then cooling to room temperature. Extension occurred in the presence of 10 U exonuclease-deficient (exo-) Klenow DNA polymerase (New England Biolabs,

Beverly, MA) and addition of all four deoxynucleoside triphosphates to the extension mixture (0.14 mM final concentration). As discussed above, α -thio dATP was substituted for dATP to prevent interference with the luciferase reaction. After extension, the contents of each well were serially diluted for comparison of light emission as a function of PPi concentration.

[00259] In an exemplary embodiment, extension and real-time luminometric monitoring were performed at 25°C in an IVIS™ imaging system (Xenogen, Alameda, CA) or in and Lmax™ microplate luminometer (Molecular Devices, Sunnyvale, CA). A luminometric reaction mixture was added to the substrate with different concentrations of extended primed single-stranded DNA or self primed oligonucleotide. The luminometric assay mixture (40 μ l) contained 3 μ g luciferase (Promega, Madison, WI), 50 mU recombinant ATP sulfurylase (Sigma Chemicals, St. Louis, MO), 0.1 M Tris-acetate (pH 7.75), 0.5 mM EDTA, 5 mM Mg-acetate (Sigma Chemicals), 0.1% (w/v) bovine serum albumin (Sigma), 2.5 mM dithiothreitol (Sigma), 10 μ M adenosine 5'-phosphosulfate (APS) (Biolog, Alexis Biochemicals, Carlsbad, CA), 0.4 mg polyvinylpyrrolidone/ml (molecular weight 360000) and 100 μ g D-luciferin/ml (BioThema AB, Haninge, Sweden). Emitted light was detected in real-time and measured after approximately 45 seconds with 1 second and 10 second integration times for the CCD imaging system and luminometer, respectively. FIG. 13 shows a Xenogen image and amplified signal output for a 0.1 picomole sample of pathogen nucleic acid. Similar images have been obtained with pathogen nucleic acid samples as low as 0.1 attomole. Note that using the modified protocol with 0.01 attomole to 10 attomole purified pyrophosphate or ATP added, the background light intensity is essentially zero. FIG. 14 shows an increase in steady state light emission from a 10 fmol sample analyzed by BRC. FIG. 14 shows that even in the presence of random noise background that is of approximately the same order of magnitude as the actual signal, the pyrophosphate induced signal can still be detected as a shift in the baseline level of the light output.

[00260] The light coupling efficiencies of each system (including path loss) from the microtiter plate where the DNA samples were located to the sensor were approximately 0.012% and 8% for the CCD and PMT systems, respectively. In the CCD imaging system, a 96-well microtiter plate with multiple DNA samples was placed 18 cm below the lens of the camera, and in the

luminometer a 384-well microtiter plate was inserted in the instrument chamber, where a PMT directly moves into close proximity (1 cm) of the sample for reading.

Detection Devices

[00261] The photosensitive device is typically either in direct proximity of the BRC reaction to directly receive incident photons, or relatively far from the buffer with a light coupling device (e.g. optical fiber or mirror system) capable of directing light from the sample to the detector. In an exemplary embodiment, a UDT-PIN-UV-50-9850-1 photodiode (Hamamatsu Corp., Hamamatsu, Japan) was used with a transimpedance amplifier with a gain of 10^8 volts/amp.

Example 2: Detection of Pathogen Nucleic Acids by BRC

[00262] Detection of pathogen nucleic acids by BRC assay was performed as described in Example 1, using a cooled CCD camera for light measurements. The signal obtained from 10 attomole to 100 femtomole of selected target cells or pathogens was determined. The target cells or pathogens, comprising either a synthesized oligonucleotide-loop or a 230 bp PCR product, were detected in 40 μ l reaction volumes (FIG. 15). The same type of study was done using a standard luminometer. The performance of the two systems with a modified integration time (1 sec in CCD and 10 sec in luminometer) was compared (FIG. 15 and FIG. 16). These studies demonstrated the ability to detect 1 amol to 100 amol of target in 20 μ l for both the oligonucleotide-loop and the 230 bp PCR product (MBP) with the luminometer.

[00263] The sensitivity of 1 amol observed in the BRC assay corresponds to approximately one million free pyrophosphate molecules in the solution, which is an extremely low concentration for 20 μ l. If a given target DNA sequence has an extendable length of 1000 base pairs (which is a conservatively low number), then the disclosed sensitivity should allow detection of 1000 target DNA molecules (and 100 target pathogen cells) using a single specific primer. Additional variations of the BRC assay, such as enhanced BRC, provide even higher sensitivity.

Example 3: Detection of Pathogen Nucleic Acids by Real-Time PCR Using BRC

[00264] The BRC assay was performed using real-time quantitative PCR (RT-PCR) methods, in comparison with standard RT-PCR (Taqman™ assay, Applied Biosystems, Foster City, CA). A dilution series of cDNA from *S. invicta* Queen GP-9B was quantified using RT-PCR with the Taqman™ assay and BRC. As shown in FIG. 17, the sensitivity of BRC was better than

Taqman™, using one tenth of the starting material and 10 less PCR cycles. The end point measurement sensitivity of BRC, based on the above result is at least 1000 better than the fluorescence based Taqman™ RT-PCR method.

Example 4: Measurement of Endogenous ATP Content by BRC

[00265] In certain embodiments of the invention, the amount of cells or microorganisms in a sample may be quantified by assaying for endogenous ATP and/or PPi. In an exemplary embodiment, the relative number of cells present was determined by employing BRC detection with samples comprising a dilution series of cell lysates from U937 macrophages (FIG. 18a) or *E. coli* (FIG. 18b). Even when diluted to a point where there was (on average) lysate from only one cell present, the BRC assay showed a detectable signal above background (FIG. 18). This indicates that the BRC detection assay can determine the presence of as few as 1-10 cells (equivalent to a few million total ATP molecules). More generally, BRC based ATP and/or PPi detection may be used to quantify anywhere from 1 to 10,000 cells or microorganisms.

Example 5: SNP detection Using Total RNA Templates

[00266] SNPs have been detected by hybridization of total RNA incubated with gene specific or allele specific primers and/or probes (Higgins *et al*, *Biotechniques* 23:710-714, 1997; Newton *et al*. *Lancet* 2:1481-1483, 1989; Goergen *et al*, *J Med Virol* 43:97-102, 1994; Newton *et al*, *Nucleic Acids Res* 17:2503-2516, 1989). Using the methods disclosed herein, SNPs may be detected by BRC, using sequence specific extension primers designed to bind to the template with the 3' end of the primer located over the base of interest (SNP site) (FIG. 15). In preferred embodiments, the primer sequence is selected so that the end of the primer to which nucleotides will be attached is base-paired with the polymorphic site.

[00267] In certain embodiments, where the SNP is located in a coding sequence, the primer may be allowed to hybridize to total RNA or polyadenylated mRNA. (Alternatively, to detect non-coding SNPs genomic DNA or PCR amplified genomic DNA may be used as the target.) The template/primer fragments are used as the substrate for a primer extension reaction (*e.g.*, Sokolov, *Nucleic Acids Res* 18:3671, 1989) in the presence of reverse transcriptase. If a target sequence is present that is complementary to the sequence specific primer, extension occurs and pyrophosphate is generated. An aliquot of the reaction product is added to a BRC reaction

mixture as disclosed above. Extension products (PPi) are detected as disclosed above, allowing identification of the SNP in the pathogen nucleic acid.

[00268] Typically SNPs exist in one of two alternative alleles. The allelic variant of the SNP may be identified by performing separate BRC reactions with primers specific for each of the SNP variants. In an alternative embodiment, the SNP allele may be identified using a gene specific primer that binds immediately upstream of the SNP site, allowing extension to occur in the presence of a single type of dXTP (or α -thio dATP) (FIG. 15). Extension will occur if the added dXTP is complementary to the SNP nucleotide.

Example 6: SNP Detection Using cDNA Templates

[00269] In alternative embodiments, SNPs may be detected from cDNA templates. Complementary DNAs may be prepared by standard methods, as disclosed above, and hybridized with gene specific or allele specific primers (FIG. 15) in 20 mM Tris-HCl (pH 7.5), 8 mM MgCl₂ or other standard conditions. The primers are designed to bind to the template with the 3' end located over the polymorphic position. The template/primer fragments are then used as substrates in a primer extension reaction, as discussed above. Pyrophosphate generation, detected by the BRC reaction, indicates the presence of a SNP sequence that is complementary to the primer. As discussed above, gene specific primers also may be used in combination with single dXTPs.

Example 7: Pathogen Typing by BRC

[00270] FIG. 16 illustrates embodiments of the invention in which BRC can be used to identify, type and/or quantify target pathogens in a sample. Total RNA or genomic DNA of the pathogenic organism may be incubated with pathogen specific primers (FIG. 16). In some embodiments, a single primer may be specific for one type of pathogen, or may be specific for a family of pathogens. Alternatively, multiple primers specific for different sub-types of a family of pathogens may be used. After hybridization in a suitable buffer, primer extension occurs with either reverse transcriptase or DNA polymerase, as disclosed above. The presence of a target pathogen type, or a member of a family of pathogens, is detected by luminescence using BRC. The pathogen titer (number of pathogenic organisms) in the sample may be determined by photon integration over a time interval, as discussed above.

Example 8: Pathogen Typing by Rolling Circle

[00271] In various embodiments, BRC may be performed using a rolling circle replication process (FIG. 17). In this case, a circular primer sequence is allowed to hybridize with either total RNA or genomic DNA, for example of a pathogen. (Banér *et al*, *Nucleic Acids Research*, 26:5073-5078, 1998). As discussed above, the primer may be specific for a single type of pathogen, or may react with a family of pathogenic organisms. Alternatively, multiple circular primers specific for different members of a family of pathogens may be used. After hybridization, an exonuclease is added to the solution. The exonuclease digests single-stranded RNA or DNA, leaving intact double stranded RNA or DNA. The double stranded nucleic acid acts as the substrate in a primer extension reaction as discussed above, using reverse transcriptase or DNA polymerase. Formation of PPi is monitored by BRC.

Example 9: Isothermal or Thermal Amplification of Nucleic Acids and BRC

[00272] A variety of nucleic acid amplification methods can be used in combination with cell or pathogen detection. Genomic DNA, cDNA, mRNA or total cell RNA may be extracted, mixed with appropriate reagents for amplification and, for example, BRC reagents for detection and quantification in the same tube. In certain embodiments, the amplification step may be performed separately from detection and quantification.

Polymerase Chain Reaction (PCR) Amplification

[00273] Genomic DNA is extracted, combined with dNTP, Mg, buffer, Taq Polymerase enzyme and sequence specific primers. The samples are cycled through 1-30 rounds of denaturation at 95°C, annealing at 40-70°C and extension at 72°C. An aliquot of the PCR amplified sample is added to BRC assay mix and the amount of PPi generated quantified as a measure of the number of starting copies of sequence specific DNA present in the sample. Alternatively the PCR step can be combined with the BRC assay in one tube using a thermostable luciferase enzyme and ATP sulfurylase enzyme, as discussed above. In this method there is a coupling of amplification and detection/quantification of the target sequence. The number of PPi released in solution as a result of amplification is directly proportional to the length of the target sequence, and can be used to quantify the number of starting pathogen nucleic acid in solution.

Results

[00274] Genomic DNA was amplified with primers specific to Maltose Binding Protein (MBP). An aliquot of the PCR product was diluted serially and assayed using the BRC method. Images were taken with standard CCD sensor with 1 sec integration time (not shown). Alternatively a luminometer was used with 10 sec integration time (not shown).

[00275] BRC was used with a complex genomic background with and without amplification steps. A bacterial colony containing the Rho 52 gene in a plasmid was grown on an agar plate. A colony with less than 100,000 bacteria was isolated and placed into 4 tubes containing buffer. The tubes were heated to 95°C for 5 minutes and then the master mix containing Taq Polymerase, dNTPs, primers specific to Rho 52 and Mg was added. Tube 1 was heated to 95°C for 1 min, 55°C for 1 min and 72°C for 1 minute for one amplification cycle. Tubes 2, 3 and 4 were amplified using similar temperatures but for 10 cycles, 20 cycles, and 30 cycles, respectively. An aliquot of each was added to the BRC assay for PPi measurement. Using the disclosed methods, target DNA was detected and quantified in each tube (not shown). Reference samples had all reagents and biological substances except primers.

[00276] Other potential isothermal applications that may be combined with BRC include Ribo-SPIA (Nugen Technologies), NASBA, RCA (Amersham), Eberwine (Ambion), Invader (Third Wave Technologies) as well as cleavage based assays.

Example 10: Sequence Detection Using BRC

[00277] The BRC procedure may be used to detect a given sequence of pathogen nucleic acid.

BRC Analysis With Isothermal Amplification

[00278] BRC assay reagents and isothermal/thermal amplification reagents are added together into the tube with target sequence specific primer(s) and amplified at the appropriate temperature. Light intensity is measured for presence or absence of target sequence.

BRC Analysis With PCR

[00279] PCR reaction mixture was added to the tube contents along with a primer specific to the target sequence. The sample was subjected to one or more cycles of PCR amplification, for example at 95°C (1 min), 55°C (1 min), and 72°C (1 min). In an illustrative embodiment, PCR amplification was performed for 0, 10, 20 or 30 cycles using a RO 52 sequence inserted into a

plasmid vector. An aliquot was added to BRC reagents and light intensity was measured for presence or absence of target sequence.

Results

[00280] FIG. 18 shows that BRC can be used with a complex genomic background with and without amplification steps. Bacterial colonies containing a RO 52 sequence inserted into a standard plasmid vector were grown on an agar plate. A colony with less than 100,000 bacteria was isolated and placed into 4 tubes containing buffer. The tubes were heated to 95°C for 5 minutes and then the master mix containing Taq Polymerase, dNTP, primers specific to RO 52 and Mg (2.5 mM MgCl₂) was added. Tube 1 was heated to 95°C for 1 min, 55°C for 1 min and 72°C for 1 minute for one cycle. Tubes 2, 3 and 4 were subjected to similar temperature cycles but respectively for 10 cycles, 20 cycles, and 30 cycles. An aliquot of each was added to the BRC assay for PPi measurement. The target RO 52 insert sequence could be detected and quantified in each tube after zero, 10, 20 and 30 cycles of amplification. A reference sample containing all reagents and biological substances except the RO 52 specific primers showed no detectable signal (FIG. 18).

Example 11: Isothermal DNA Amplification Assays with BRC Detection

[00281] Amplification of specific DNA probes provides a powerful tool for the detection of infectious diseases, genetic diseases, and potentially cancer. Use of BRC detection may involve at least some amplification. PCR is the present amplification method of choice, but this is a time consuming and instrumentally-cumbersome step due to the requirement for temperature cycling. In certain preferred embodiments of the invention, isothermal methods of BRC detection may be used.

[00282] One method of isothermal BRC assay may involve simultaneous strand displacement amplification and real-time bioluminescence detection. Strand Displacement Amplification (SDA) is an *in vitro*, isothermal nucleic acid amplification technique originally based upon the ability of the restriction enzyme *Hinc* II to nick the unmodified strand of a hemiphosphorothioate form of its recognition site, and the ability of the 5'→3' exonuclease-deficient Klenow fragment of DNA polymerase I (exo- klenow) to extend the 3'-end at the nick site and displace the downstream DNA strand. Exponential amplification results from coupling sense and antisense

reactions in which strands displaced from a sense reaction serve as a target for an antisense extension reaction and vice versa (*e.g.*, Walker *et al.*, *Proc. Natl. Acad. Sci* 89:392-396, 1992).

[00283] Although effective, target generation by restriction enzyme cleavage presents a number of practical limitations. Little *et al.*, (*Clinical Chemistry* 45:777-784, 1999) disclose an alternative approach to SDA that eliminates the requirement for restriction enzyme cleavage of the target sample prior to amplification. The method exploits the strand displacement activity of *exo-* klenow to generate target DNA copies with defined 5'- and 3'-ends. The new target generation process occurs at a single temperature (after initial heat denaturation of the double-stranded DNA). The target copies generated by this process are then amplified directly by SDA.

[00284] The ability of isothermal BRC to accurately detect specific DNA target sequences is demonstrated by using two different PCR amplicons, Ro 52 DNA fragment (A) and Ro 60 DNA fragment (B), with corresponding primers for each (A' and B').

[00285] Different buffers, with different buffer capacity, different pH values, and a spectrum of ionic strength conditions are screened, in a combinatorial fashion, for their effects on the SDA and BRC reaction steps. Currently SDA amplification is performed in a mixture containing 50 mM Tris-HCl (pH 7.4), 6 mM MgCl₂, 50 mM NaCl and 50 mM KCl (9) while BRC is performed in 100 mM Tris-Acetate (pH 7.75) and 5 mM Mg-Acetate. Buffers used include Tris-acetate and Hepes-acetate buffers. The pH is varied between pH 6.5 and 8.5. The buffer concentration is varied between 0.05 M and 0.2 M. The conditions are optimized for SDA and BRC protocols.

[00286] Microwell plate wells (for placing different primer sets for individual DNA sequences) are prepared by adding primers A', B', a combination of A' and B', or an irrelevant primer set, C' into different wells to be exposed to sample mixture. The sample mixture contains the (SDA) polymerase, luciferase, ATP sulfurylase, adenosine 5'-phosphosulfate (APS), D-luciferin (BioThema) and two different target DNA molecules, A and B. A positive signal is detected only in the wells having the appropriate DNA primers with the appropriate complementary target sequence present in the sample. The sensitivity of BRC detection technology employed with SD isothermal DNA amplification is demonstrated by employing serially diluted samples of DNA primer probes. Sensitivity in the range of 0.1 amol to 1 µmol is observed.

Example 12: Portable Biosensor

[00287] Certain embodiments of the invention concern a portable, photodiode-based sensor system for ultra-sensitive detection of nucleic acid molecules. The BRC chemistry has shown a high performance in terms of sensitivity and signal level. This high gain eliminates the necessity for an expensive photodetector (e.g., a cooled CCD). Maintenance of a controlled environment in the device facilitates the reliable measurement of the photon generation rate of the assay and quantification of nucleic acid molecules. A reaction chamber with controllable temperature and minimum background light is preferred.

[00288] The detector is less expensive than current molecular detection platforms, which are often sophisticated, delicate and bulky devices that are highly labor intensive. The associated biochemical procedures are expensive, require skilled personnel, and often take days or weeks to complete. BRC in combination with the handheld device is a preferred detection system, due to its low cost and higher sensitivity. This places the device within reach of many more individual users, instead of only those with access to well-equipped core facilities. In addition, the platform enables physicians and first responders to a medical emergency to diagnose problems in a rapid, sensitive, and highly specific manner, facilitating appropriate prompt response or treatment. The device can also be used for consumer and industry-based environmental monitoring, for use in healthcare and agriculture-food sectors, and for defense and homeland security in applications requiring the detection and identification of biological agents.

Photodiode and Sensor Design

[00289] Maximization of the signal to noise ratio (SNR) of the photogenerated signal is facilitated by an understanding of photodiode and sensor parameters. Most visible light sensors comprise a 2D photodetector array, which is divided into pixels. Independent of its topology and sizing, the array contains a number of photodiodes, with a circuit as shown in FIG. 28. Photons incident on the photodiode are converted to a photocurrent, which is integrated over the capacitance C . The amount of charge collected is proportional to the light intensity and it might be clipped by saturation in high illumination. At the end of exposure time (t_{int}) the potential level is read as an electrical voltage signal (V_o) which is defined by

$$V_o = \frac{I_{ph}}{qC} \cdot t_{\text{int}} , \quad (48)$$

where q is the charge on an electron. For the BRC assay, assuming that there is 100% light collection efficiency and photodiode with unity spectral response in the emission spectra the output potential is

$$V_o = \left(\frac{t_{\text{int}}}{qC} \right) \cdot (\alpha \cdot k_L) \cdot N_{NA} \cdot (L_{NA} - L_p). \quad (49)$$

[00290] Several sources contribute to noise during the collection of the photogenerated signal. The shot noise generated during integration can be modeled as a Gaussian noise source with zero mean and variance of $(C \cdot q)^{-1} \cdot (I_{dc} + I(t)) \cdot t_{\text{int}}$. Other sources include read noise, reset noise and shot noise from background light and photodiode dark current (not considered here). The Signal-to-Noise Ratio, SNR, is defined as the ratio between the photogenerated signal power to the noise power and is given by

$$\left(\frac{S}{N} \right) = \frac{I_{ph}(t)^2 \cdot t_{\text{int}}}{q \cdot [I_{ph}(t) + I_{dc}]}. \quad (50)$$

[00291] In order to achieve a relatively high SNR, the integration time should be increased. For the design and optimization of the sensor, the following factors are taken into account: the characteristics of the amplifier, leakage currents of the devices and analog switches, and the thermal drift of the components. Furthermore, the power supply or the type of battery which drives the circuitry and electronics is chosen with care.

Temperature Control and Thermo-Electric (TE) Cooling/Heating

[00292] Peltier devices, also known as thermoelectric (TE) modules, are small solid-state devices that function as heat pumps. It is a sandwich formed by two ceramic plates with an array of small Bismuth Telluride cubes ("couples") in between. When a DC current is applied, heat is moved from one side of the device to the other, at which point it must be removed with a heat sink. The "cold" side is commonly used to cool an electronic device such as a microprocessor or a photodetector. If the current is reversed the device makes an excellent heater.

[00293] In some embodiments of the invention, TE heating is used to increase the temperature of the assay in the annealing and hybridization phase. Because Peltier devices can also be cooled by simply reversing the polarity of the current, it can also be used to decrease the temperature quickly (in contrast to typical resistive heaters).

[00294] Peltier devices may be controlled by a variety of different techniques such as pulse width modulation schemes. They can be stacked to achieve higher (or lower) temperatures, although reaching cryogenic temperatures would require great care. They are not very "efficient" and can draw amps of power. This disadvantage is more than offset by the advantages of non-moving parts, no vibration, very small size, long life, and capability of precision temperature control.

* * *

[00295] All of the COMPOSITIONS, METHODS and APPARATUS disclosed and claimed herein can be made and executed without undue experimentation in light of the present disclosure. While the compositions and methods of this invention have been described in terms of preferred embodiments, it will be apparent to those of skill in the art that variations may be applied to the COMPOSITIONS, METHODS and APPARATUS and in the steps or in the sequence of steps of the methods described herein without departing from the concept, spirit and scope of the invention. More specifically, it will be apparent that certain agents that are both chemically and physiologically related may be substituted for the agents described herein while the same or similar results would be achieved. All such similar substitutes and modifications apparent to those skilled in the art are deemed to be within the spirit, scope and concept of the invention as defined by the appended claims.